



INSTITUTE OF INFORMATION  
AND COMMUNICATION  
TECHNOLOGIES  
BULGARIAN ACADEMY OF  
SCIENCE



# Level sets and graph-cuts (Deformable models)

Centro de Visión por Computador,  
Departament de Matemàtica Aplicada i Anàlisi,  
Universitat de Barcelona



# The problems of Medical image analysis vs. Computer Vision

## Segmentation

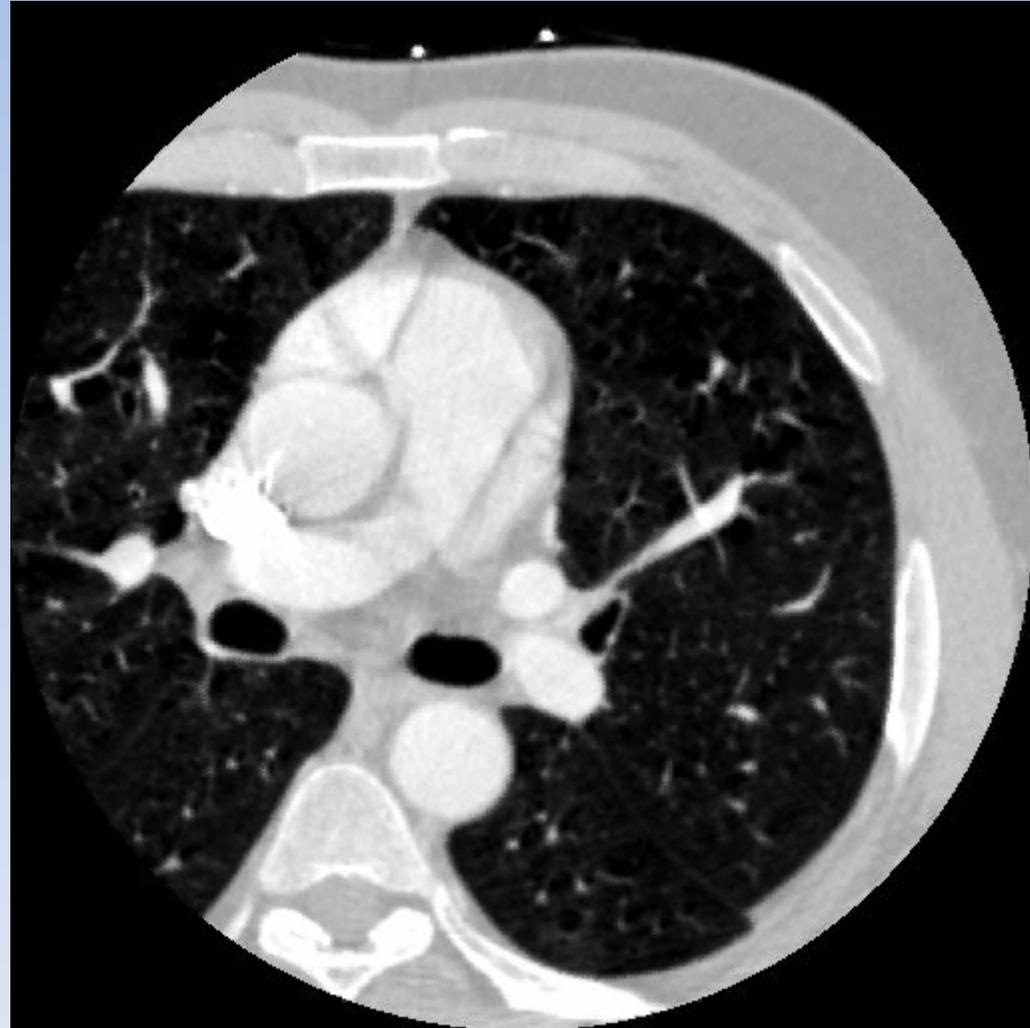
Object recognition

Atlas matching

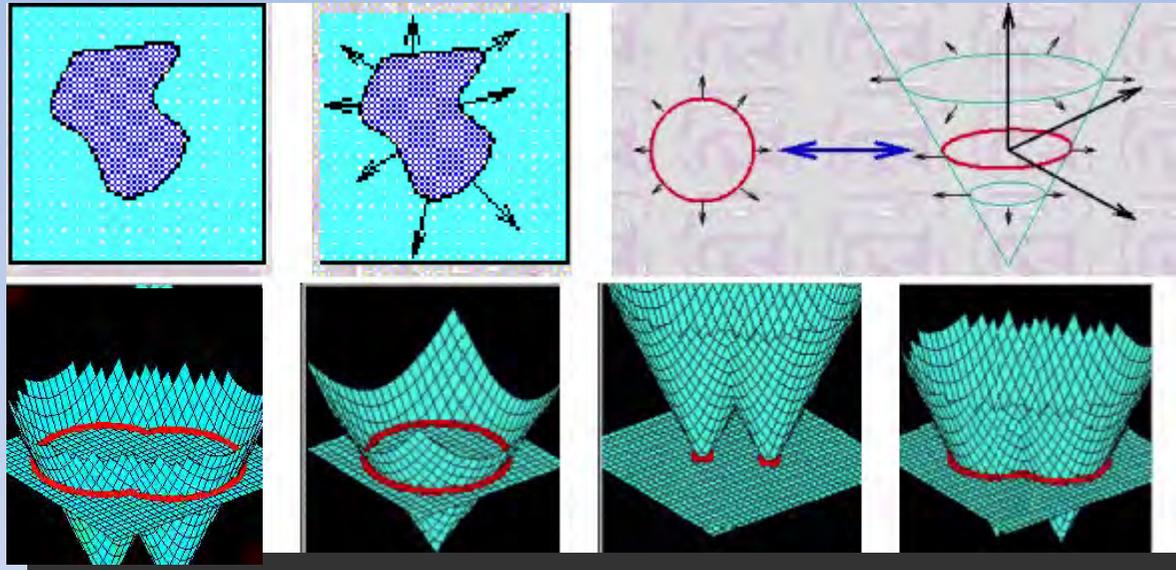
Registration

3D reconstruction

Deformation/Motion analysis



# Geodesic Active Contours (Level Sets)



Numerical techniques to track interface evolution between different regions

General time-dependent level set method

Tracking the moving boundary by the level set approach (reprint from J.A.Sethian)

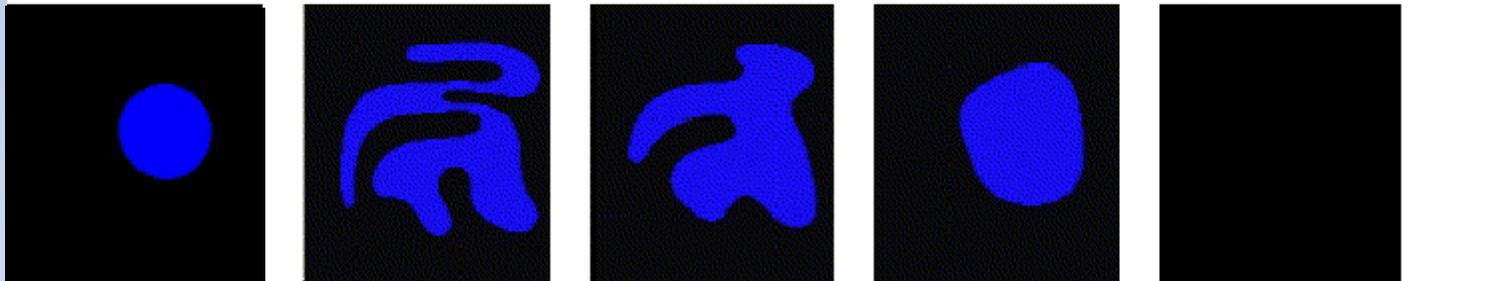
- The motion of the interface is matched with the zero level set of a level set function
  - The resulting initial value partial differential equation for the evolution of the level set function resembles a Hamilton-Jacobi equation.

From J.A.Sethian

# Motion under Curvature



Simple and not simple closed curves (reprint from J.A.Sethian)



Curve collapsing under its curvature (reprint from J.A.Sethian)

## Theorem in differential geometry:

- Any simple closed curve moving under its curvature collapses nicely to a circle and then disappears.

# Geodesic Active Contours

The energy function:

$$E(Q) = \alpha \int_0^1 |Q'(u)|^2 du + \int_0^1 g(|\nabla I(Q(u))|^2) du$$

can be represented as:

$$L_R = \int_0^{L(Q)} g(|\nabla I(Q(u))|) ds$$

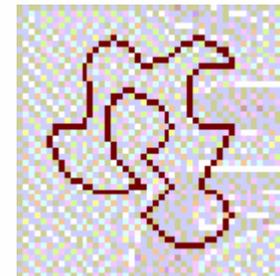
where  $s$  is the Euclidean arc-length parameter and  $g$  is a function of the image.

We are looking for a **path (curve) with minimal length definition weighted by an image component.**

**Evolution equation:** applying Euler-Lagrange of  $L_R$  to deform  $Q(0) = Q_0$  towards a minimum of  $L_R$ :

$$\frac{\delta Q}{\delta t} = g(I)k\vec{n} - (\nabla g, \vec{n})\vec{n}$$

where  $k$  is the curvature and  $\vec{n}$  is the unit inward normal.



# The Level Sets Geodesic Flow

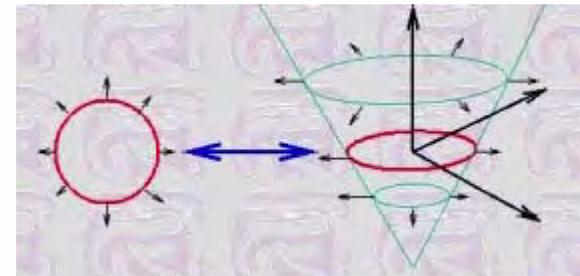
$$\frac{\delta Q}{\delta t} = g(I)k\vec{n} - (\nabla g, \vec{n})\vec{n}$$

$$\begin{aligned} \frac{\delta \phi}{\delta t} = & |\nabla \phi| \operatorname{div} \left( g(I) \frac{\nabla \phi}{|\nabla \phi|} \right) + cg(I) |\nabla \phi| = \\ & g |\nabla \phi| \operatorname{div} \left( \frac{\nabla \phi}{|\nabla \phi|} \right) + (\nabla g, \nabla \phi) + cg(I) |\nabla \phi| \end{aligned}$$

i.e. the level sets move according to:  $Q_t = g(I)(c+k)\vec{n} - (\nabla g, \vec{n})\vec{n}$

**Stopping criteria:**

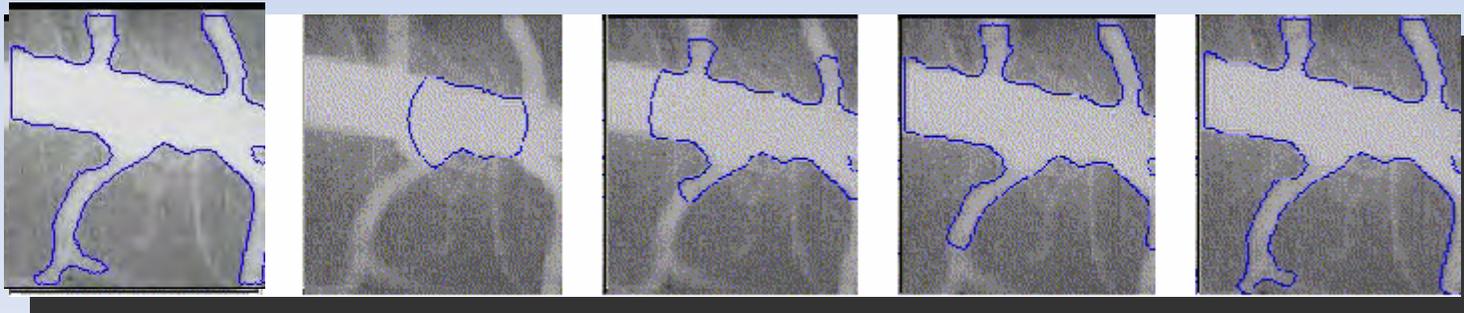
$$g = \frac{1}{1 + |G * \nabla I|^p}$$



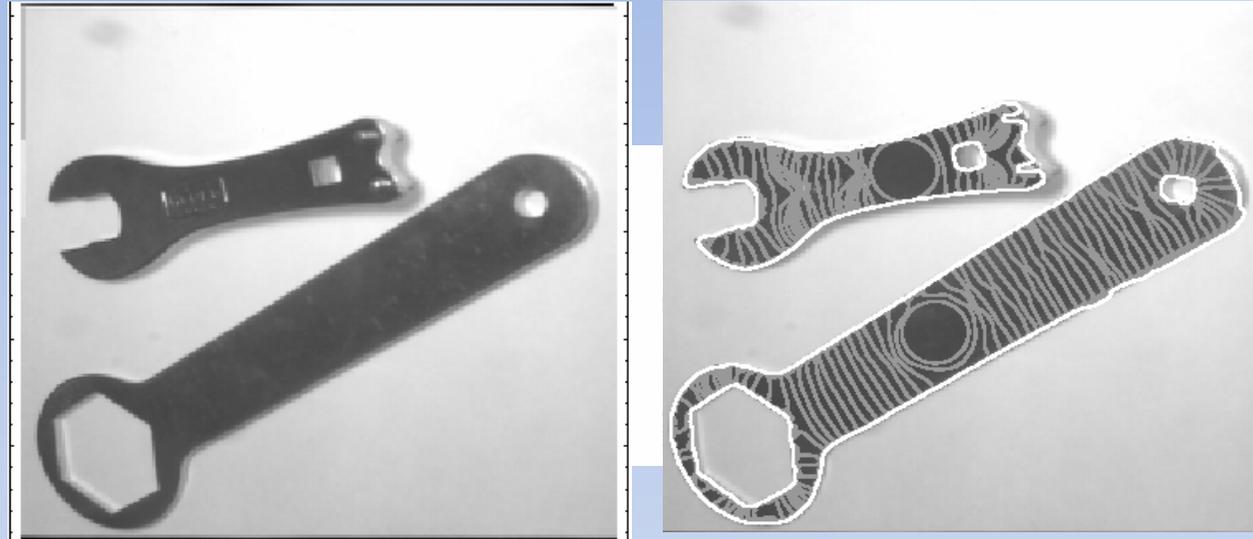
# Level Set Methods for Shape Recovery

## The key idea:

- to evolve the curve outwards with a speed depending of the curvature and the image
  - quickly expand when passing over places with small image gradient
  - slow down when crossing large image gradient places



# Segmentation by Geodesic Snakes



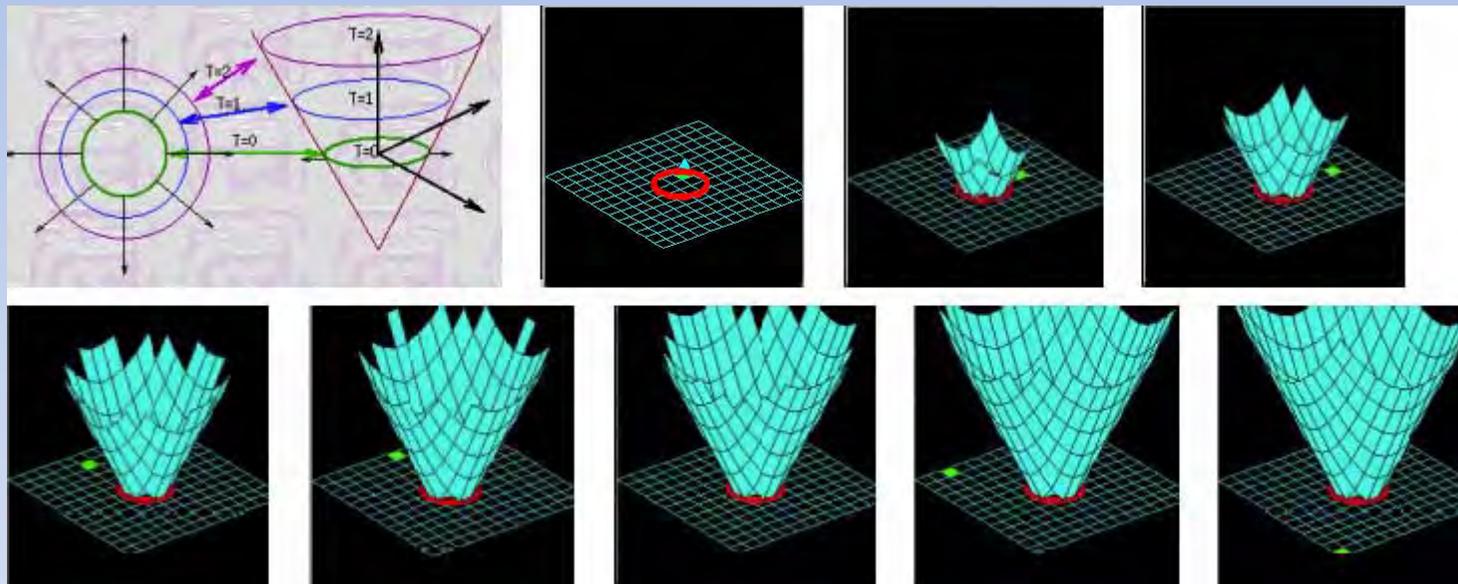
Outward motion to detect close objects. The initial contour is given by the image frame

## Advantages

- The level set approach allows the evolving front to change topology, break and merge.
- Almost no change in case of surface extraction.
- Existence, uniqueness, stability and convergence of the solution of evolution equation are proved.

From V. Casselles

# The Fast Marching Method



- Construction of stationary level set solution (reprint from J.A.Sethian)
  - The fast marching level set method solves the general static Hamilton-Jacobi equation applied to a convex non-negative speed function.

# Robotic Navigation with Constraints

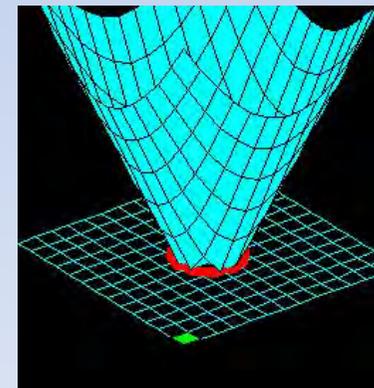
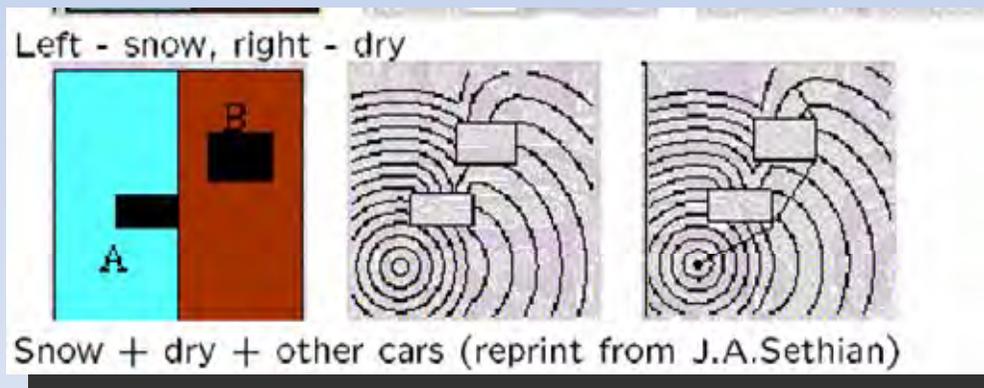
Straight line, expanding front and trace back to find path  
 Left - snow, right - dry  
 Finding the shortest path  
 Snow + dry + other cars (reprint from J.A.Sethian)

# The Fast Marching for the Global Minimum of Active Contours

## Paths of minimal action

$$U(p) = \inf_{Q_{L \rightarrow p}} \left\{ \int_Q P(Q) + \alpha \left| \frac{\delta Q}{\delta s} \right|^2 ds \right\}$$

define a *surface of minimal action*  $U$  starting at  $p_0 = Q(0)$ . The value of  $U$  is the minimal energy integrated along a path starting at  $p_0$  and ending at  $p$ .



# The Fast Marching for the Global Minimum of Active Contours

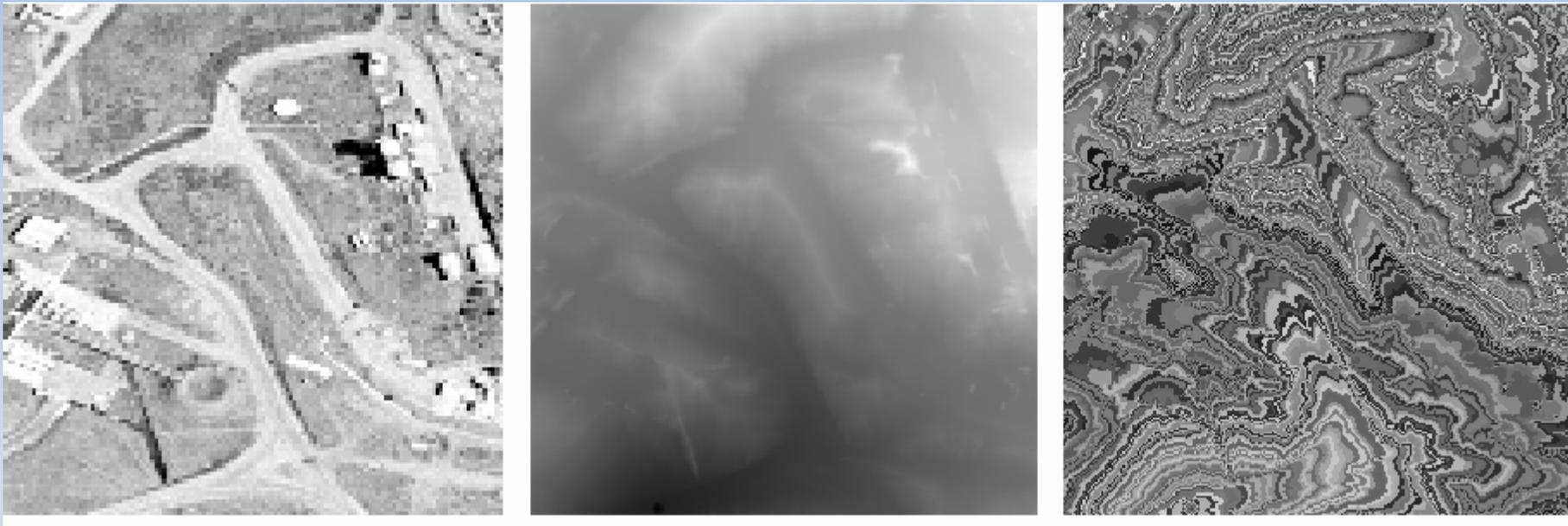
**The minimal action level sets evolution:**  $\frac{\delta L(r,t)}{\delta t} = \frac{1}{P(Q) + \alpha|Q'|} \vec{n}(r,t)$

- describes the set of equal energy contours  $L$  in 'time' where  $t$  is the value of the energy:  $\{L(r,t), r \in I\} = \{p \in R^2 | U_0(p) = t\}$ ,  $t$  - value of the energy



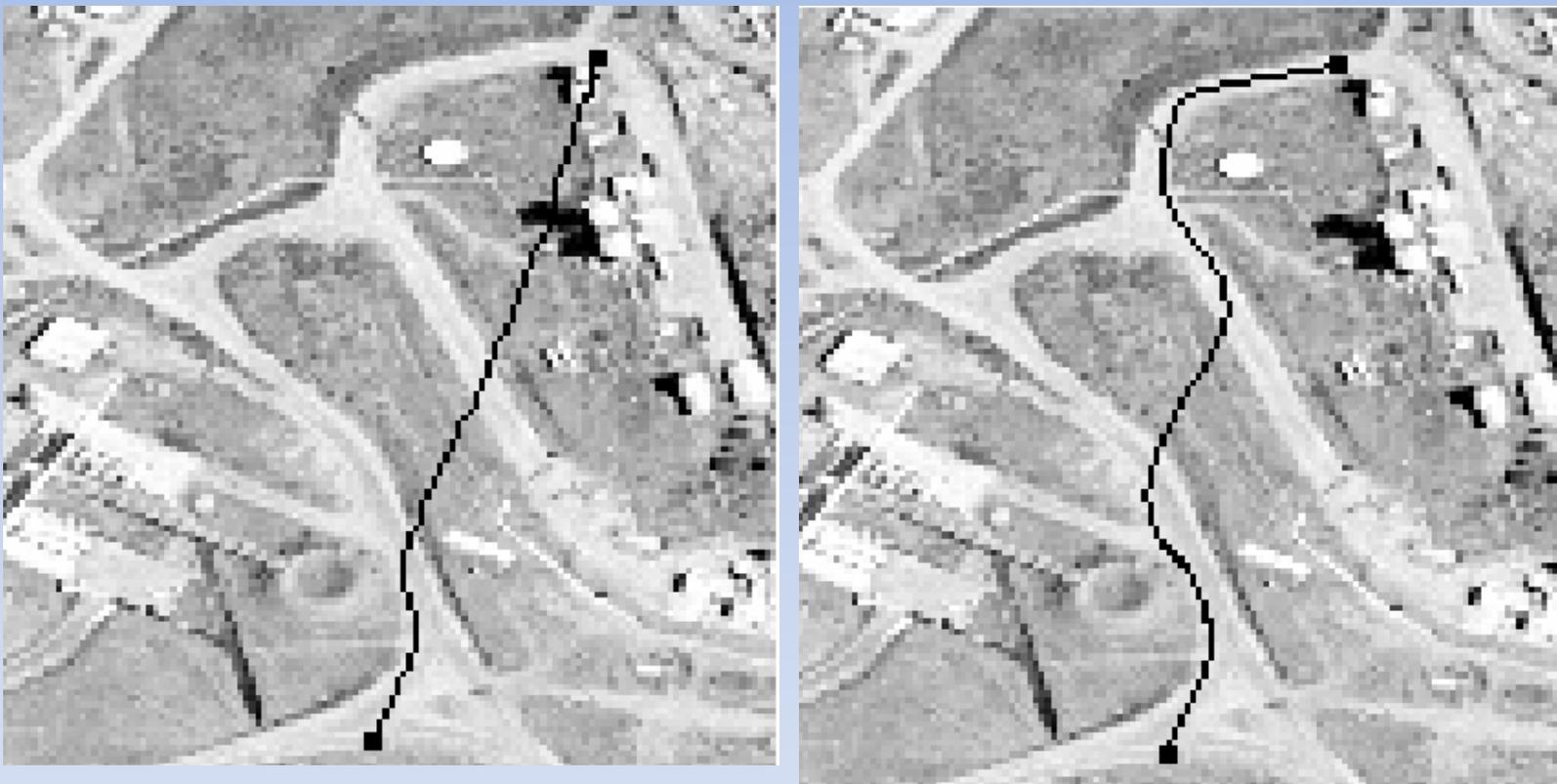
Line image: original image potential and the minimal path (reprint from L. Cohen, 1996)

# Geodesic snakes



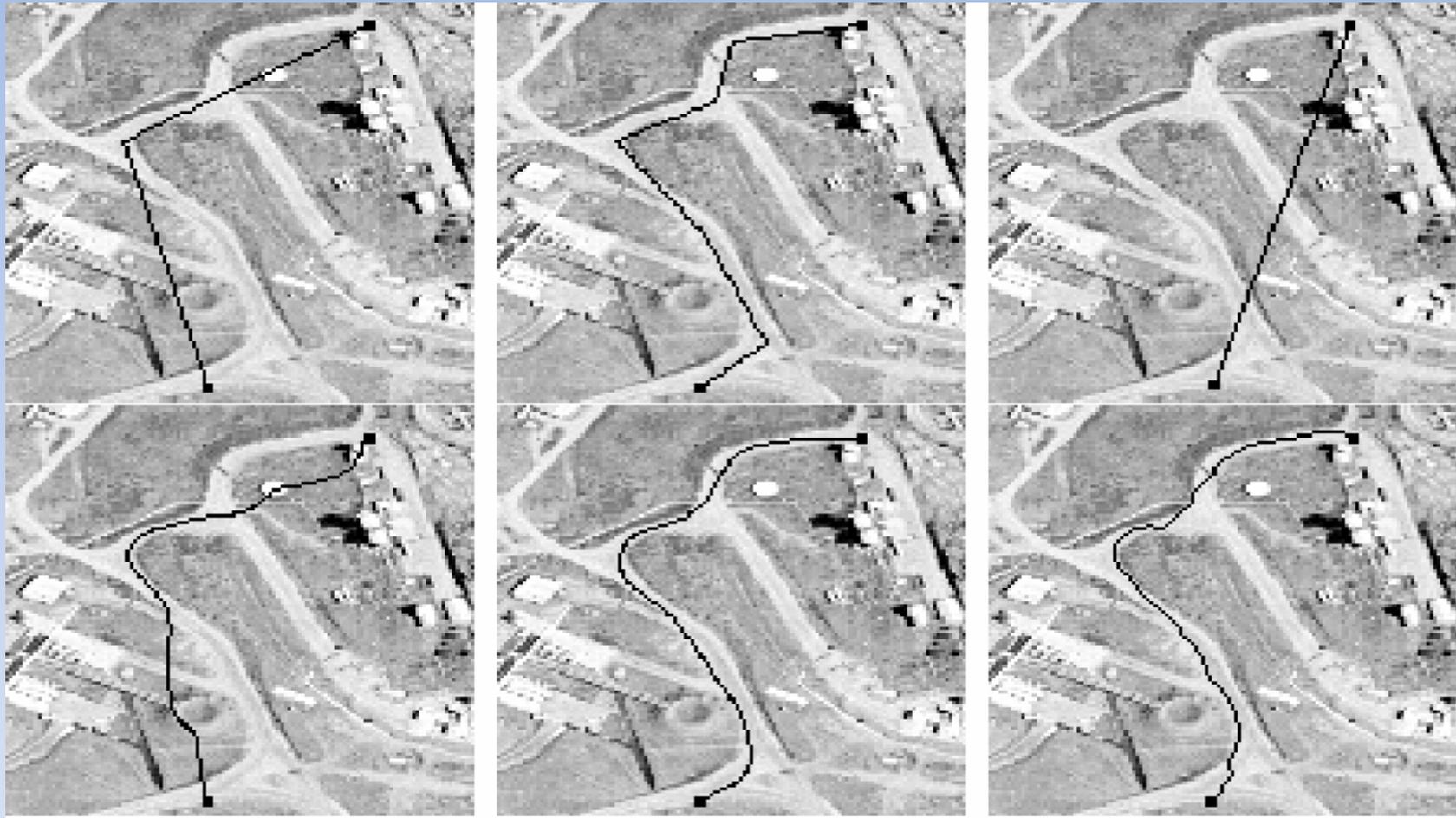
Original image and minimal action surface (in grey levels and rendered level sets)

# Classical snakes



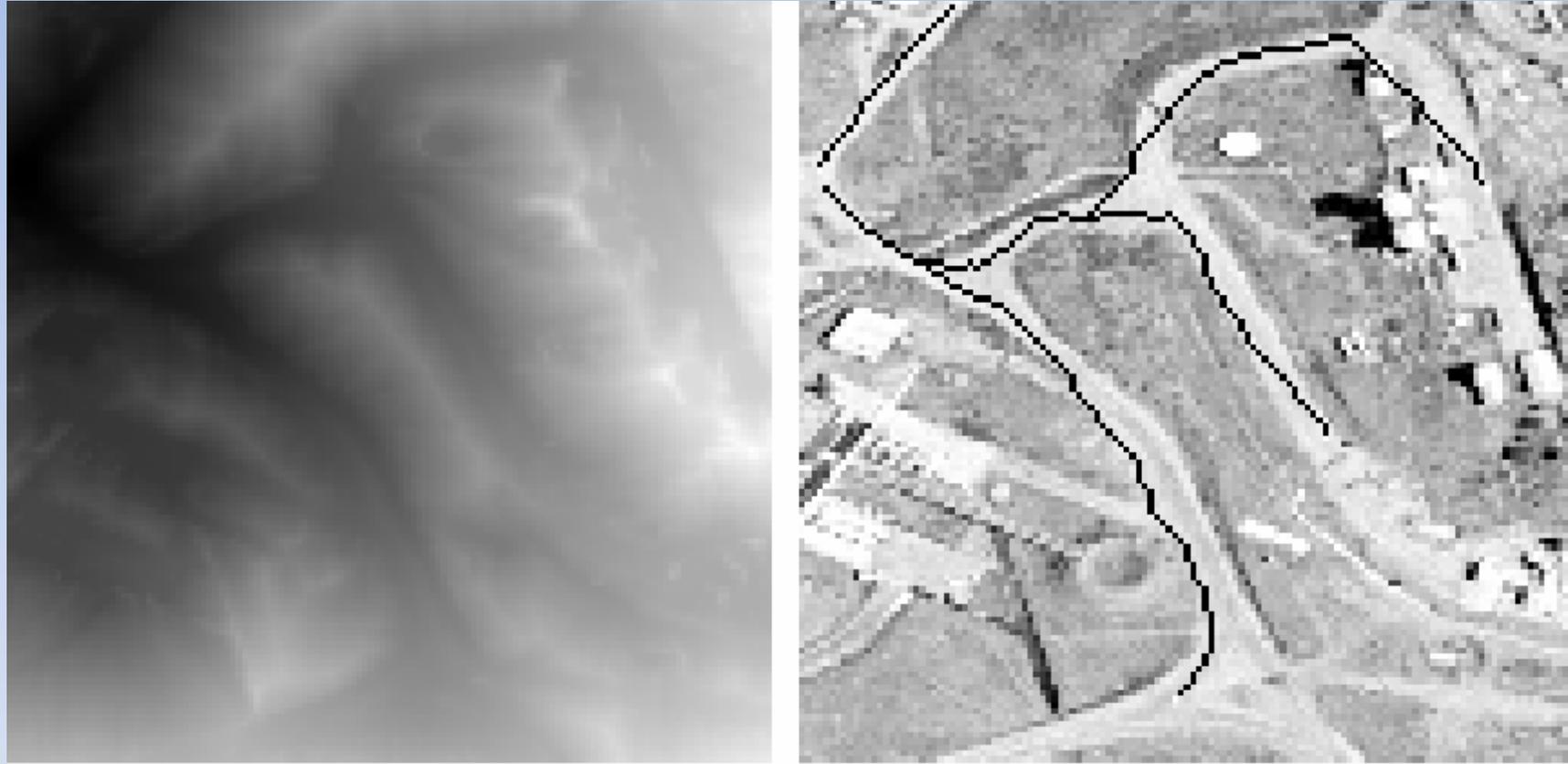
Initial snake and segmentation result by classic snakes

# Geodesic snakes



Initial snake and segmentation result by classic and geodesic snakes

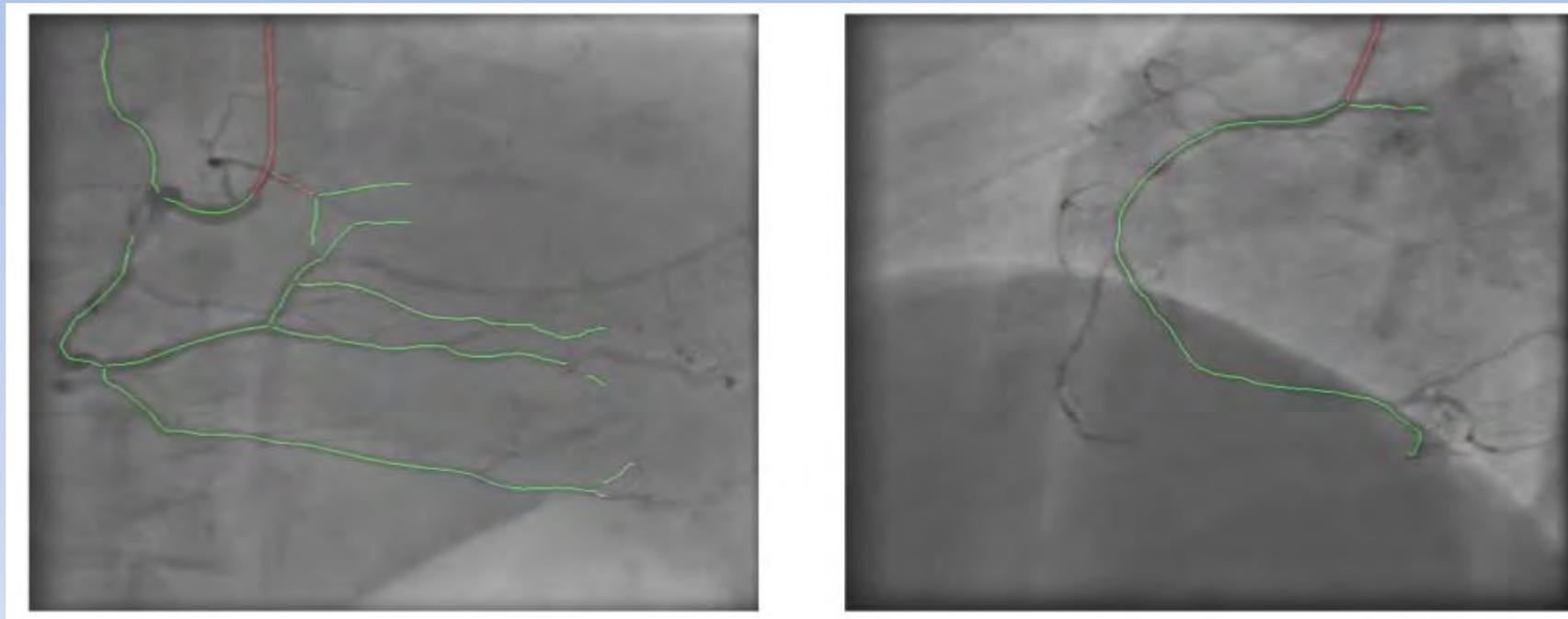
# Multiple solutions of segmentation by geodesic snakes



Minimal path between multiple points (reprint from L. Cohen, 1996)

# Application of Fast Marching for Artery detection in Angiograms

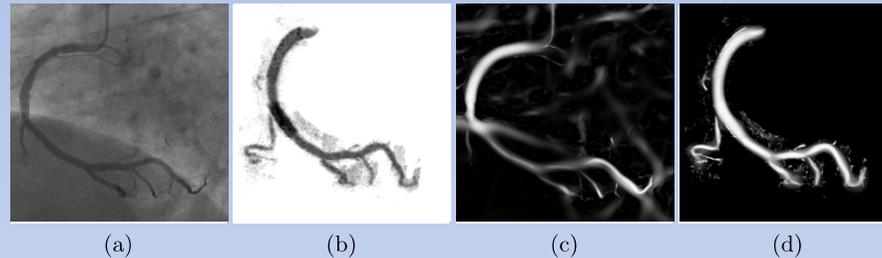
## Accurate segmentation of 2D fluoroscopy and catheter guide detection



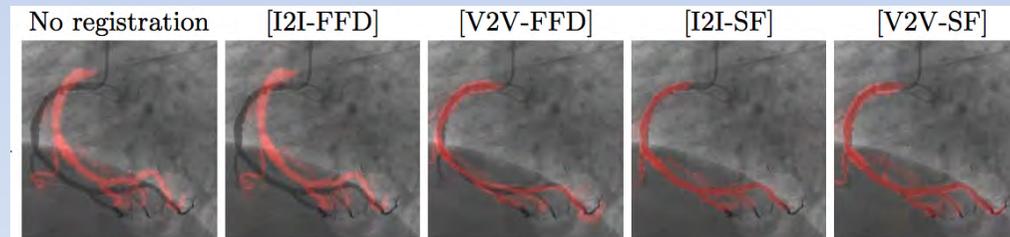
Pixels detected as catheter are shown in red. Green lines represent the vessel's centerlines as delineated automatically by the proposed method.

# Application of Fast Marching for Artery detection in Angiograms

## Development of physics-based registration techniques for 3D to 2D registration based on projective geometry



An X-Ray image (a), a simulated X-Ray image using the segmented 3D CTA coronary artery (b), and the respective Vesselness maps (c-d).

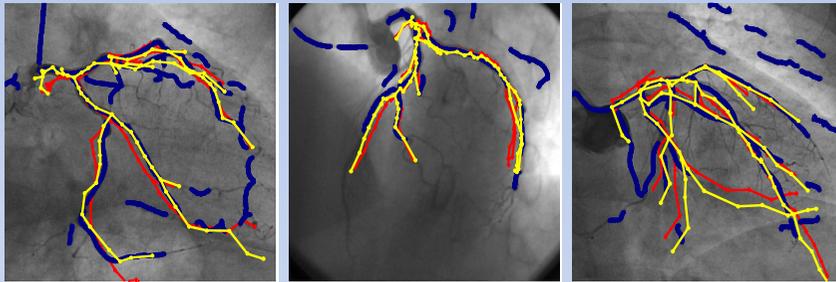


An example of successful non-rigid registration using several different pre-processing steps on the fluoroscopic image prior to registration. The red artery is the result of projecting the segmented 3D CT data.

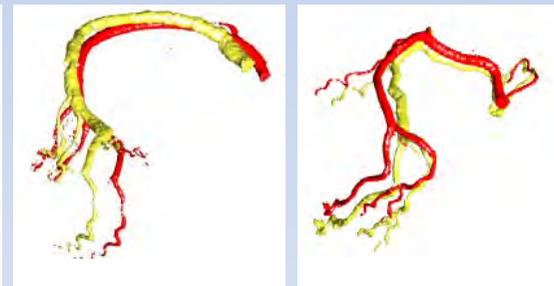
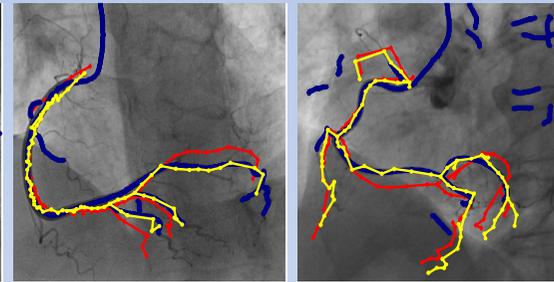
# Application of Fast Marching for Artery detection in Angiograms

Development of physics-based registration techniques for 3D to 2D registration based on projective geometry

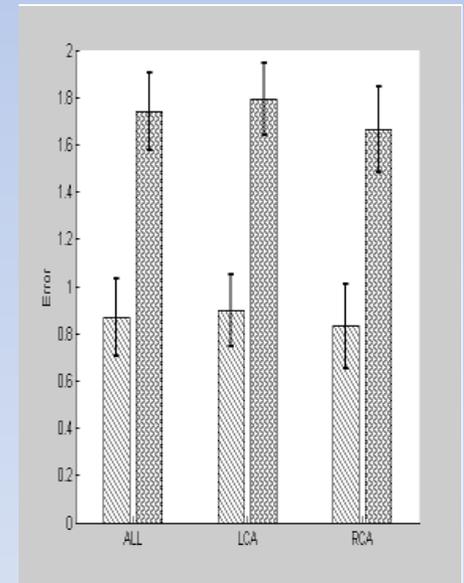
Left Coronary Artery



Right Coronary Artery



2D Reprojection Error



Reconstruction results on real vessel structures

# Advantages of level sets

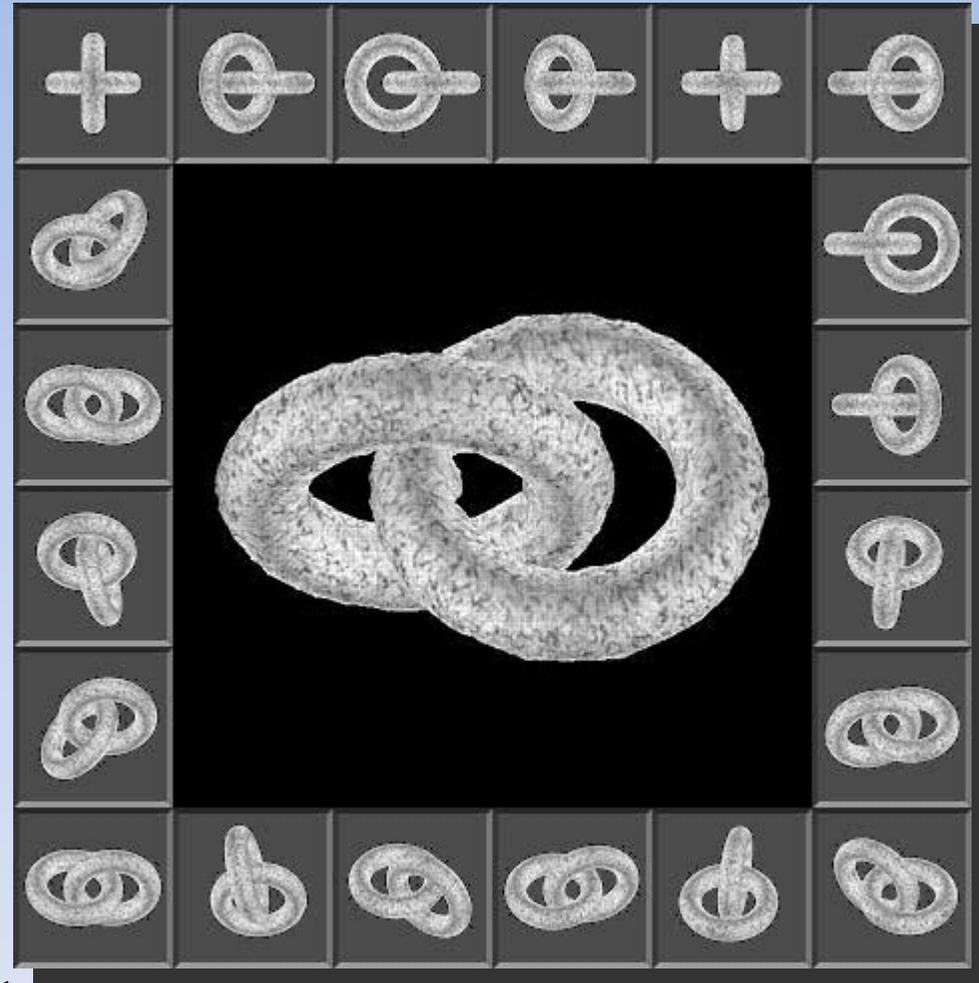
+ Topologically invariant segmentation

+ Invariant to the parameterization

- Need for good stopping criterion

+ Fast marching assures global energy minimum

- Needs initial and final point



# How to introduce high-level knowledge to regularize the segmentation problem?

- Similar pixels properties
- **General high-level constraints**
  - Snakes: contour smoothness (snakes, level sets).
  - Level sets: contour smoothness, topologically invariant.
  - **Graph cut:** connectivity and compactness of edge pixels, location and number of objects in images
- Model-guided segmentation and recognition

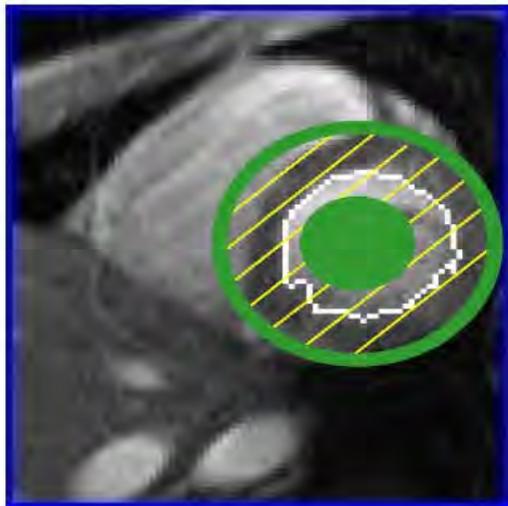


# Segmentation by Graph Cuts

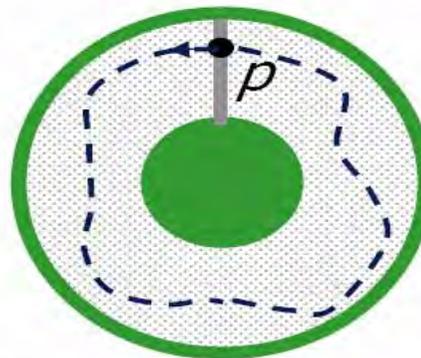
1D Graph cut  $\Leftrightarrow$  shortest path on a graph

## Example:

find the shortest closed contour in a given domain of a graph

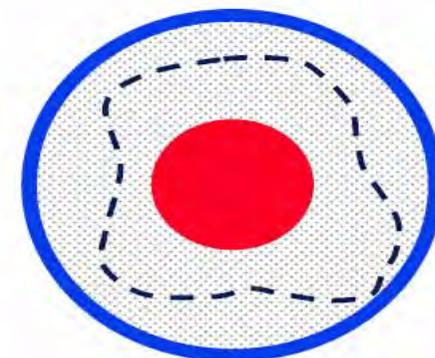


Shortest paths approach



Compute the *shortest path*  $p \rightarrow p$  for a point  $p$ . Repeat for all points on the gray line. Then choose the optimal contour.

Graph Cuts approach



Compute the *minimum cut* that separates red region from blue region

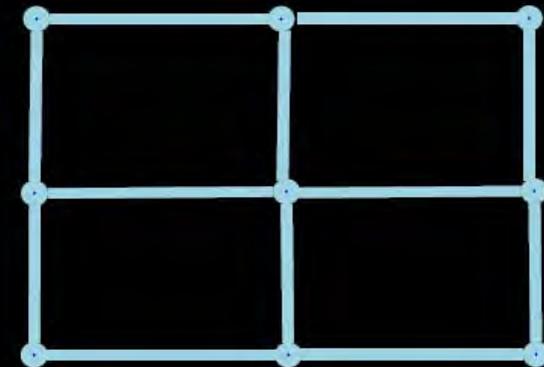
# Segmentation by Graph Cuts

 $E(X)$ 

Image (D)

$$E: \{0, 1\}^n \rightarrow \mathbb{R}$$
$$0 \rightarrow fg$$
$$1 \rightarrow bg$$

$n = \text{number of pixels}$

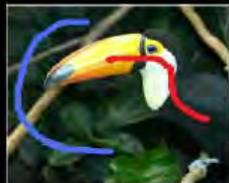
 $x_i$  $x_j$ 

[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# Segmentation by Graph Cuts

$$E(X) = \sum c_i x_i$$

Pixel Colour



Unary Cost ( $c_i$ )

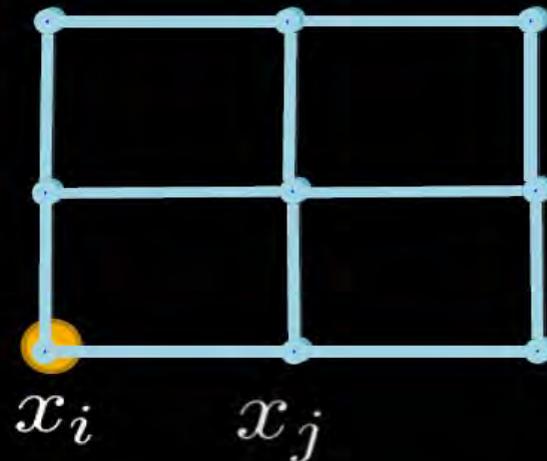
Dark (negative)    Bright (positive)

$$E: \{0, 1\}^n \rightarrow \mathbb{R}$$

$$0 \rightarrow fg$$

$$1 \rightarrow bg$$

$n$  = number of pixels



[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# Segmentation by Graph Cuts

$$E(\mathbf{X}) = \sum c_i x_i$$

Pixel Colour



Unary Cost ( $c_i$ )

Dark (negative)    Bright (positive)

$$E: \{0, 1\}^n \rightarrow \mathbb{R}$$

$$0 \rightarrow fg$$

$$1 \rightarrow bg$$

$n$  = number of pixels



$$\mathbf{x}^* = \arg \min E(\mathbf{x})$$

[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# Segmentation by Graph Cuts

$$E(\mathbf{X}) = \sum c_i x_i + \sum d_{ij} |x_i - x_j|$$

Pixel Colour

Smoothness Prior

$$E: \{0, 1\}^n \rightarrow \mathbb{R}$$

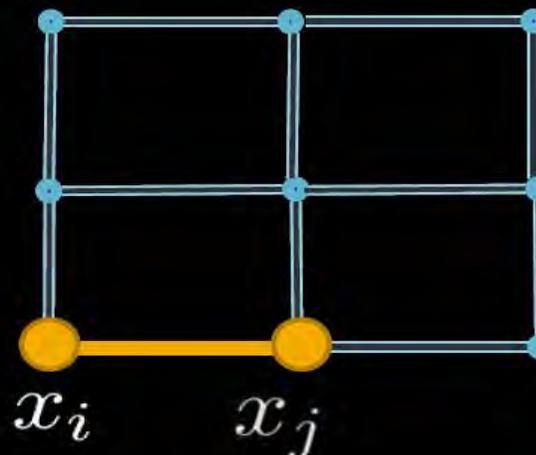
$$0 \rightarrow fg$$

$$1 \rightarrow bg$$

$n = \text{number of pixels}$



Discontinuity  
Cost ( $d_{ij}$ )



[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# Segmentation by Graph Cuts

$$E(\mathbf{X}) = \sum c_i x_i + \sum d_{ij} x_i (1-x_j) + d_{ij} x_j (1-x_i)$$

Pixel Colour

Smoothness Prior

$$E: \{0,1\}^n \rightarrow \mathbb{R}$$

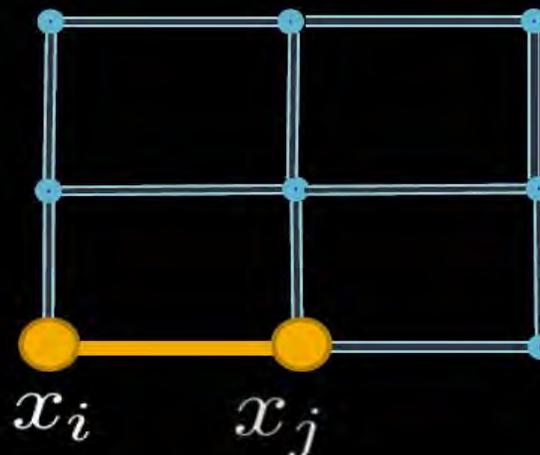
$$0 \rightarrow fg$$

$$1 \rightarrow bg$$

$n$  = number of pixels



Discontinuity  
Cost ( $d_{ij}$ )



[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# Segmentation by Graph Cuts

$$E(\mathbf{X}) = \sum c_i x_i + \sum d_{ij} x_i (1-x_j) + d_{ij} x_j (1-x_i)$$

Pixel Colour

Smoothness Prior

$$E: \{0,1\}^n \rightarrow \mathbb{R}$$

$$0 \rightarrow fg$$

$$1 \rightarrow bg$$

$n$  = number of pixels



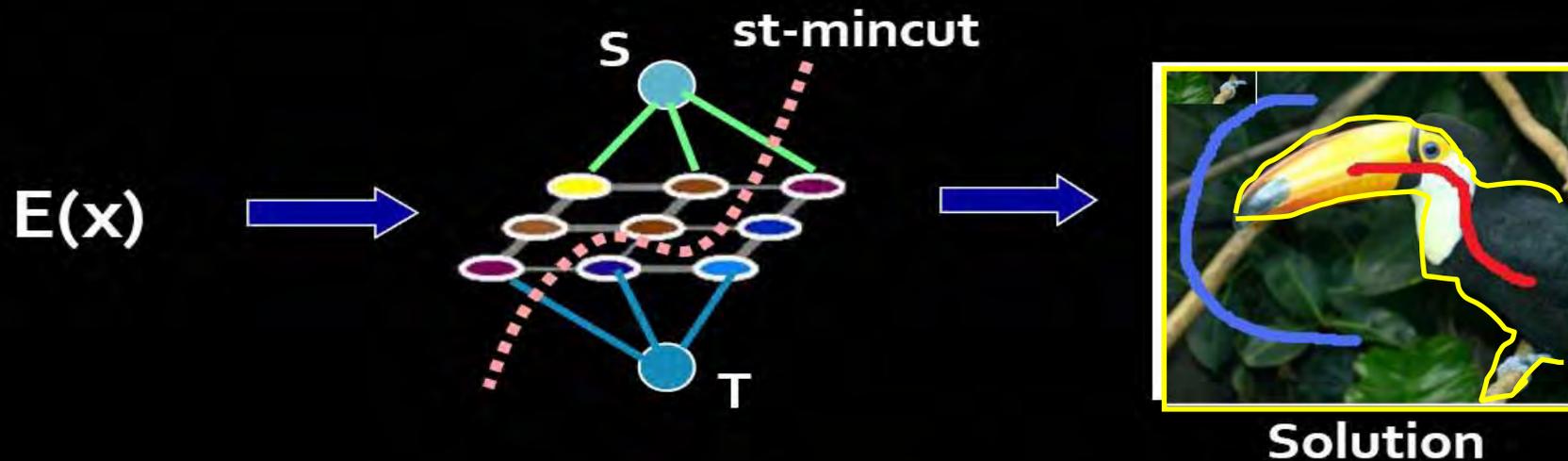
$$\mathbf{x}^* = \arg \min E(\mathbf{x})$$

[Boykov and Jolly '01] [Blake et al. '04] [Rother, Kolmogorov and Blake '04]

# So how does it work?

Construct a graph such that:

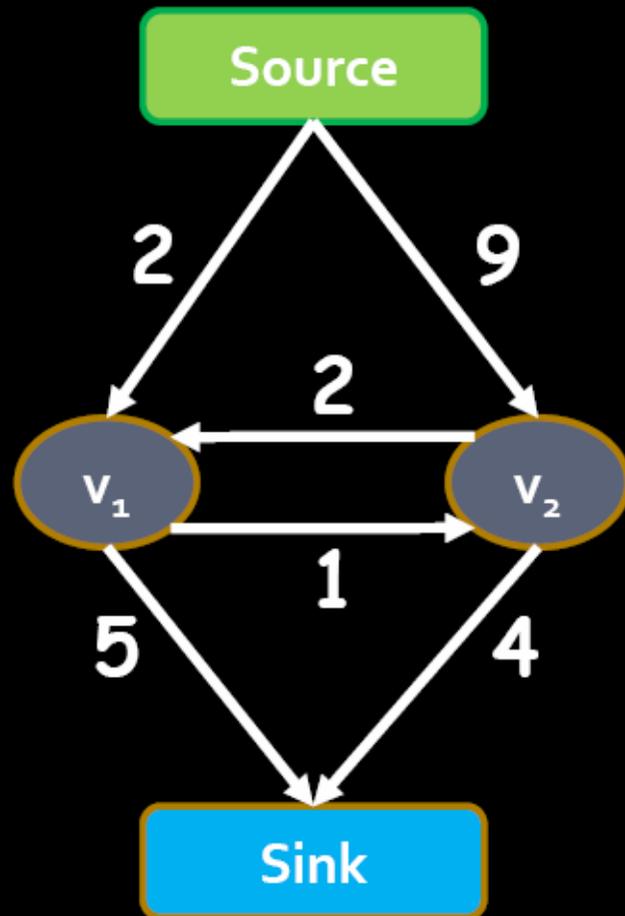
1. Any *st*-cut corresponds to an assignment of  $x$
2. The cost of the cut is equal to the energy of  $x$  :  $E(x)$



$$E(X) = \underbrace{\sum c_i x_i}_{\text{Pixel Colour}} + \underbrace{\sum d_{ij} x_i (1-x_j) + d_{ij} x_j (1-x_i)}_{\text{Smoothness Prior}}$$

[Hammer, 1965] [Kolmogorov and Zabih, 2002]

# The st-Mincut Problem



**Graph  $(V, E, C)$**

Vertices  $V = \{v_1, v_2 \dots v_n\}$

Edges  $E = \{(v_1, v_2) \dots\}$

Costs  $C = \{c_{(1,2)} \dots\}$

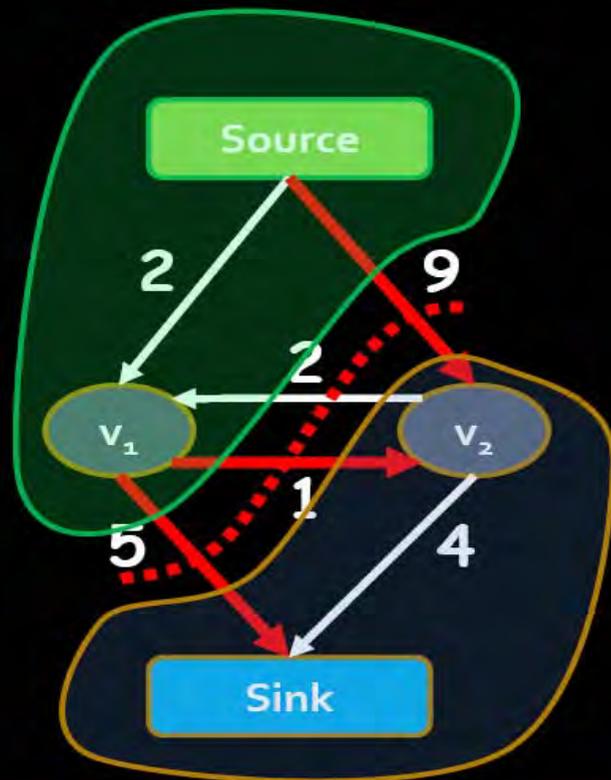
# The st-Mincut Problem

## What is a st-cut?

An st-cut  $(S, T)$  divides the nodes between source and sink.

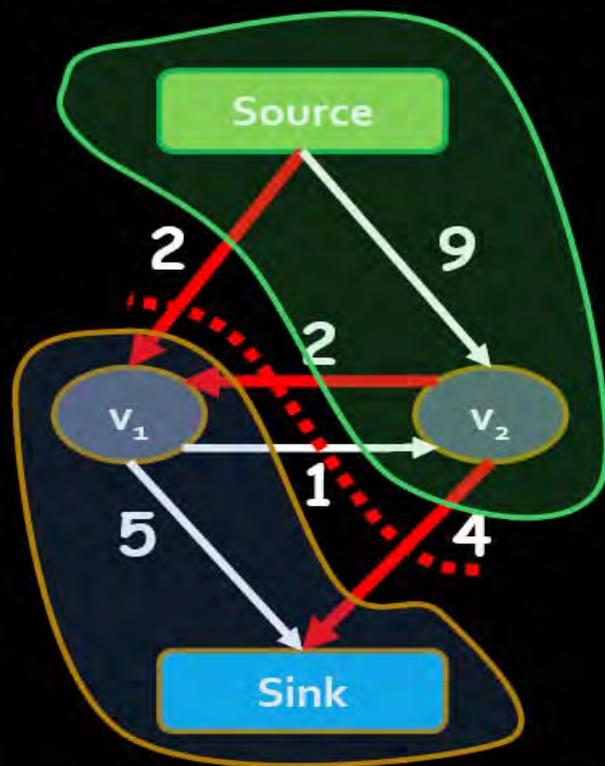
## What is the cost of a st-cut?

Sum of cost of all edges going from  $S$  to  $T$



$$5 + 1 + 9 = 15$$

# The st-Mincut Problem



$$2 + 2 + 4 = 8$$

An st-cut  $(S, T)$  divides the nodes between source and sink.

**What is the cost of a st-cut?**

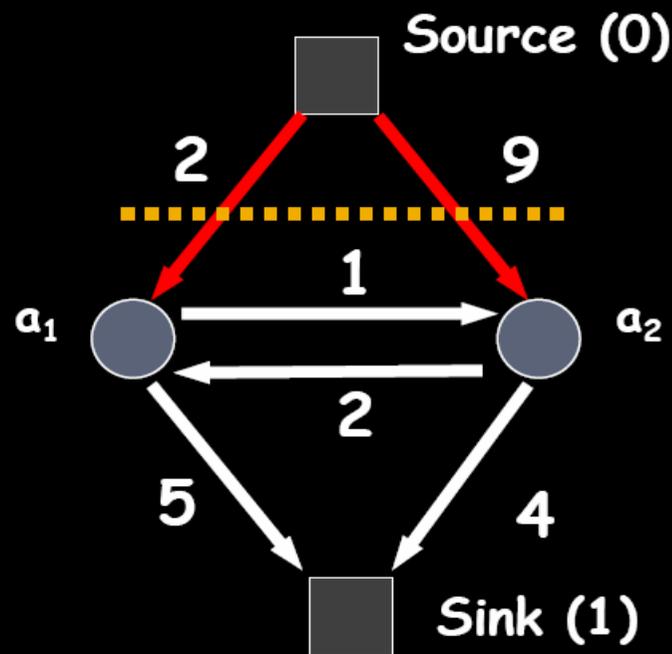
Sum of cost of all edges going from  $S$  to  $T$

**What is the st-mincut?**

st-cut with the minimum cost

# Graph construction

$$E(a_1, a_2) = 2a_1 + 5\bar{a}_1 + 9a_2 + 4\bar{a}_2 + 2a_1\bar{a}_2 + \bar{a}_1a_2$$



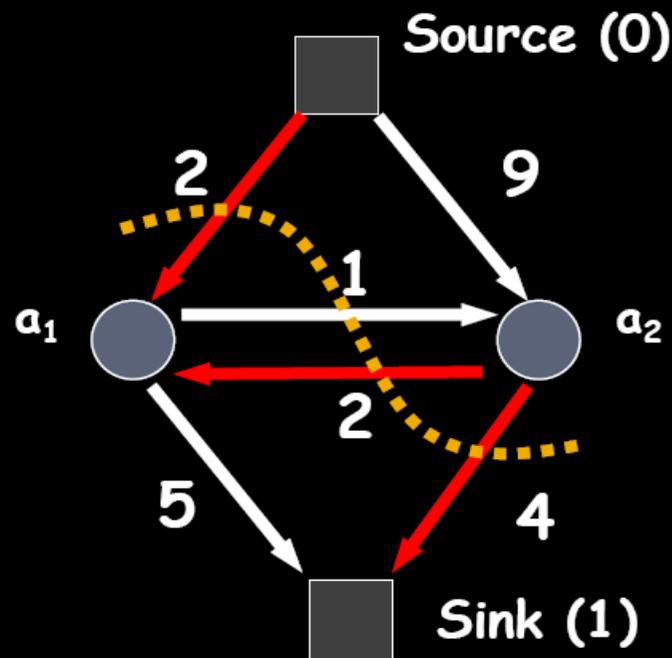
Cost of cut = 11

$$a_1 = 1 \quad a_2 = 1$$

$$E(1, 1) = 11$$

# Graph construction

$$E(a_1, a_2) = 2a_1 + 5\bar{a}_1 + 9a_2 + 4\bar{a}_2 + 2a_1\bar{a}_2 + \bar{a}_1a_2$$



st-mincut cost = 8

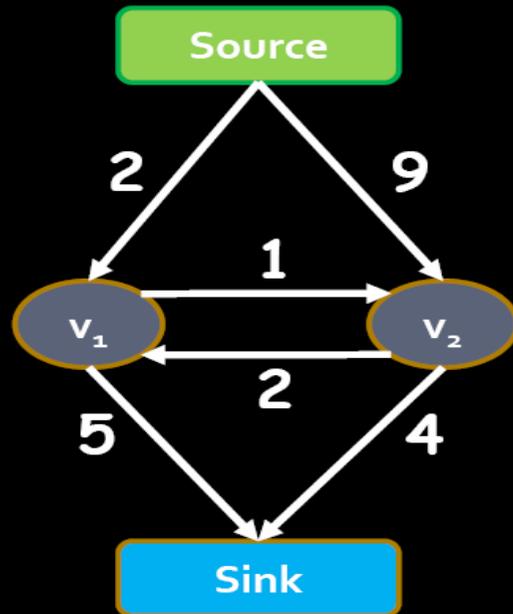
$$a_1 = 1 \quad a_2 = 0$$

$$E(1, 0) = 8$$

# How to compute the st-Mincut?

Solve the dual maximum flow problem

Compute the maximum flow between Source and Sink s.t.



Edges: Flow < Capacity

Nodes: Flow in = Flow out

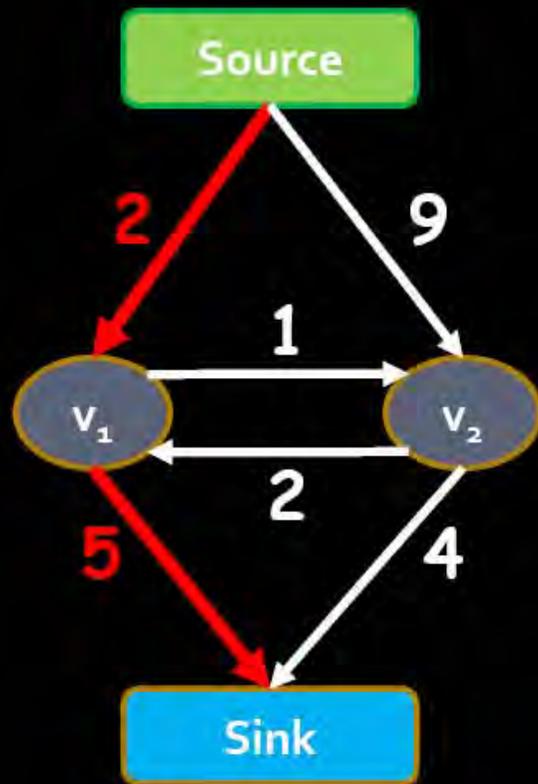
## Min-cut \ Max-flow Theorem

In every network, the maximum flow equals the cost of the st-mincut

**Assuming non-negative capacity**

# Maxflow algorithm

Flow = 0

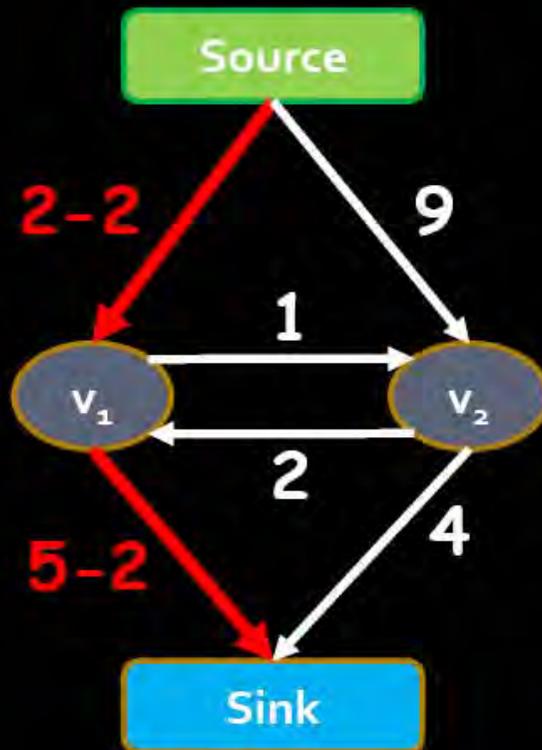


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity

# Maxflow algorithm

Flow = 0 + 2

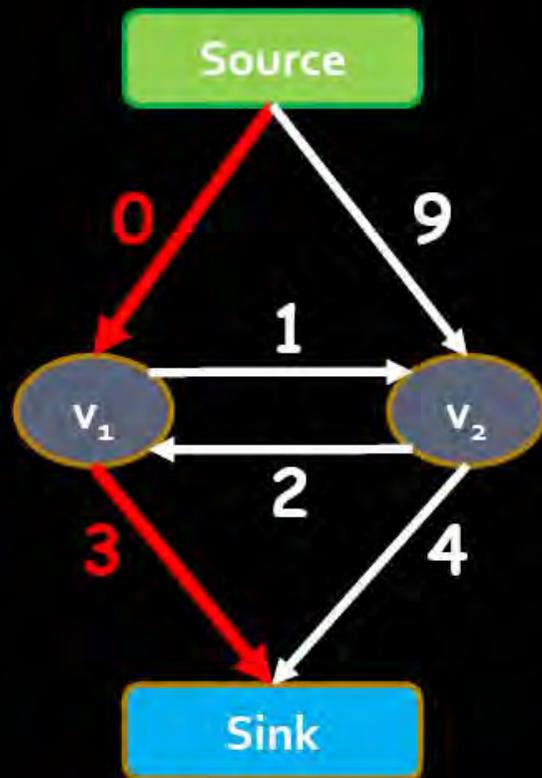


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path

# Maxflow algorithm

Flow = 2

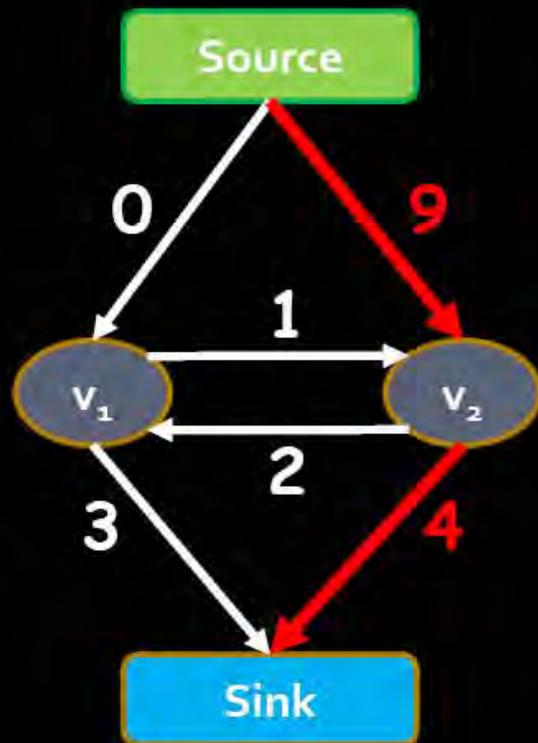


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path

# Maxflow algorithm

Flow = 2

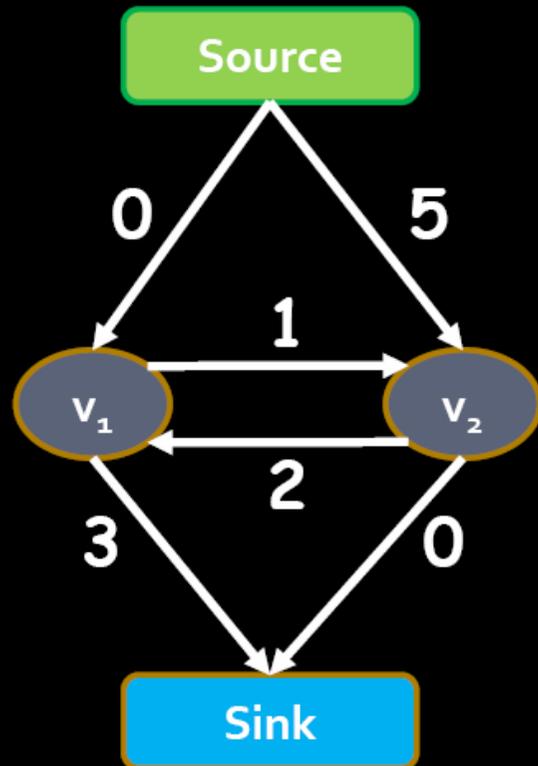


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Maxflow algorithm

Flow = 6

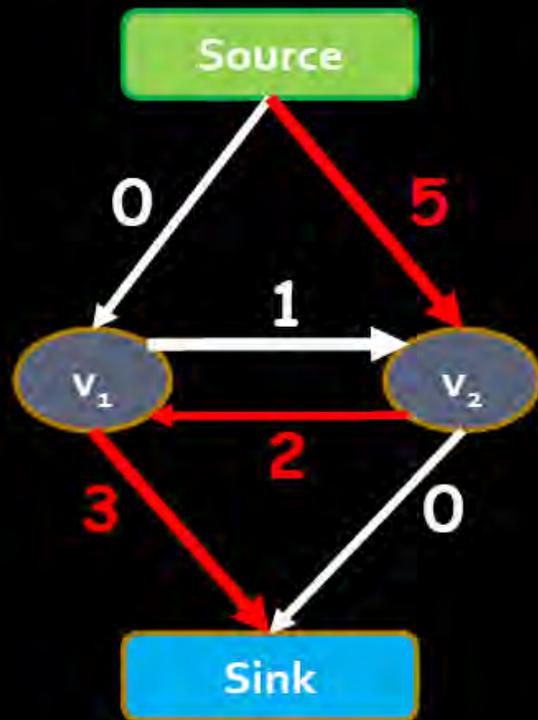


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Maxflow algorithm

Flow = 6

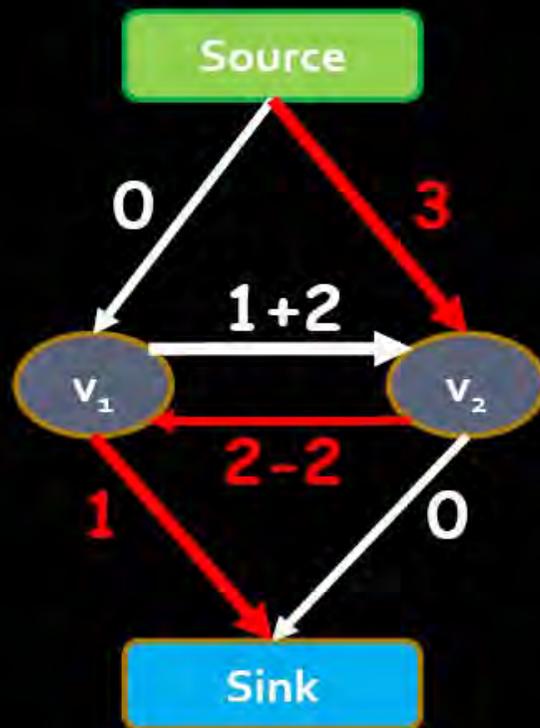


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Maxflow algorithm

Flow = 6 + 2

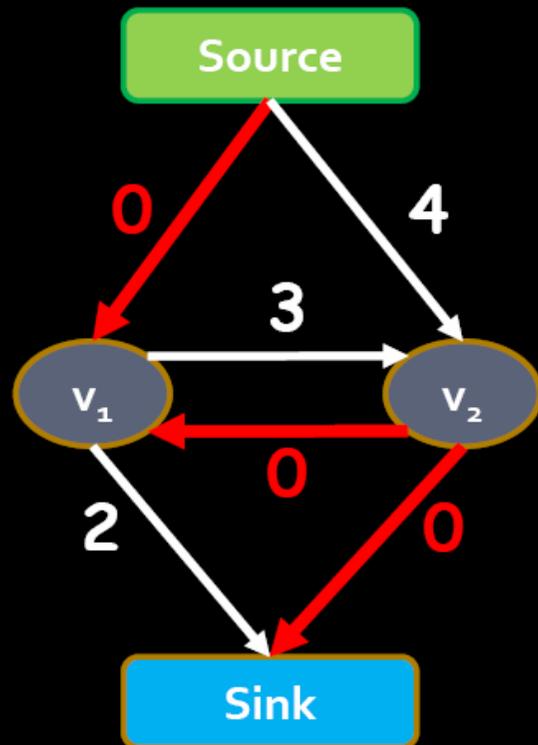


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Maxflow algorithm

Flow = 8

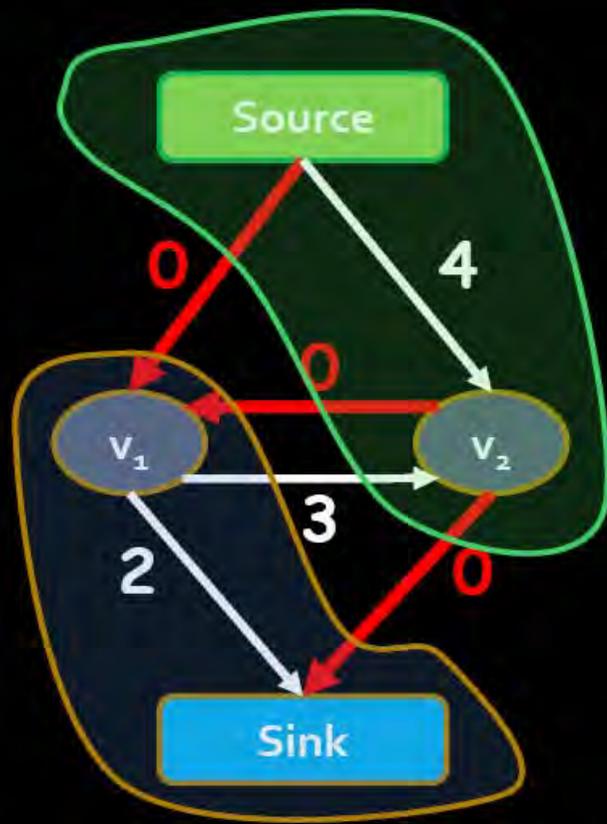


## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Maxflow algorithm

Flow = 8



## Augmenting Path Based Algorithms

1. Find path from source to sink with positive capacity
2. Push maximum possible flow through this path
3. Repeat until no path can be found

# Grab-cut

- Semi-automatic segmentation



*Ferrari, V. , Marin-Jimenez, M. and Zisserman, A.*

- Energy minimization scheme

$$E(L) = \underbrace{\sum_{p \in \mathcal{P}} D_p(L_p)}_{\text{Likelihood based on image cues}} + \underbrace{\sum_{(p,q) \in \mathcal{N}} V_{p,q}(L_p, L_q)}_{\text{Spatial coherence based on pixel relationships}}$$

Likelihood based on  
image cues

Spatial coherence based  
on pixel relationships

45

# Grab-cut

- Energy function

$$E(\underline{\alpha}, \mathbf{k}, \underline{\theta}, \mathbf{z}) = U(\underline{\alpha}, \mathbf{k}, \underline{\theta}, \mathbf{z}) + V(\underline{\alpha}, \mathbf{z})$$

Pixel differences  
based on RGB  
Euclidean distance

$$V(\underline{\alpha}, \mathbf{z}) = \gamma \sum_{(m,n) \in \mathcal{C}} [\alpha_n \neq \alpha_m] \exp(-\beta \|z_m - z_n\|^2)$$

RGB

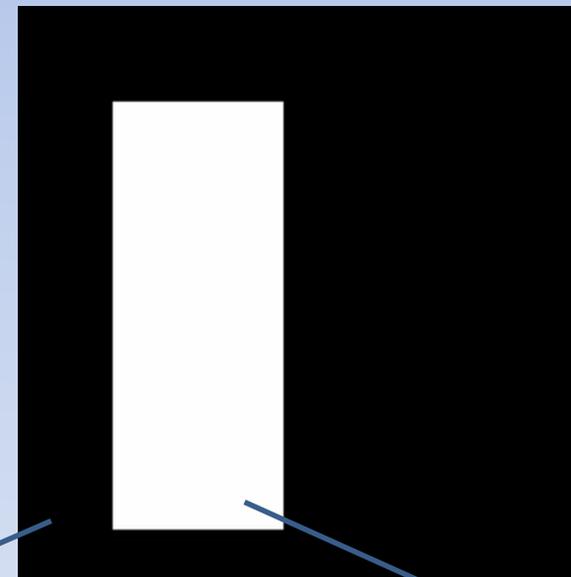
GMM  
modelling

Assign pixels  
to GMM  
components

Segmentation  
(min-cut)

[3] C Rother, V Kolmogorov, A Blake. "Grabcut: Interactive foreground extraction using iterated graph cuts", *ACM Transactions on Graphics*, 2004.

# GrabCut example

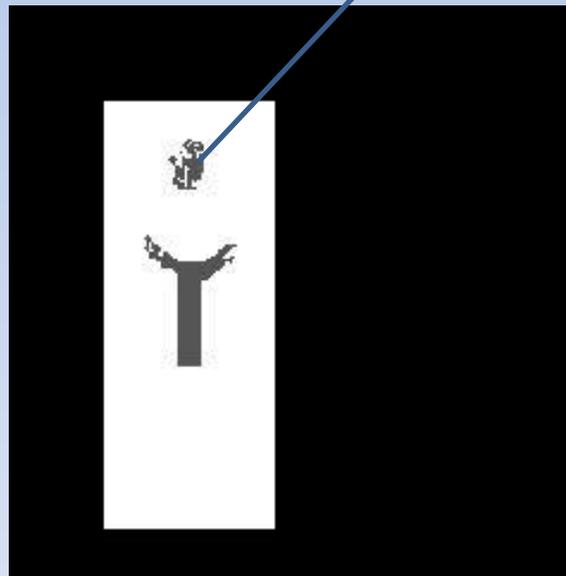


Background seeds

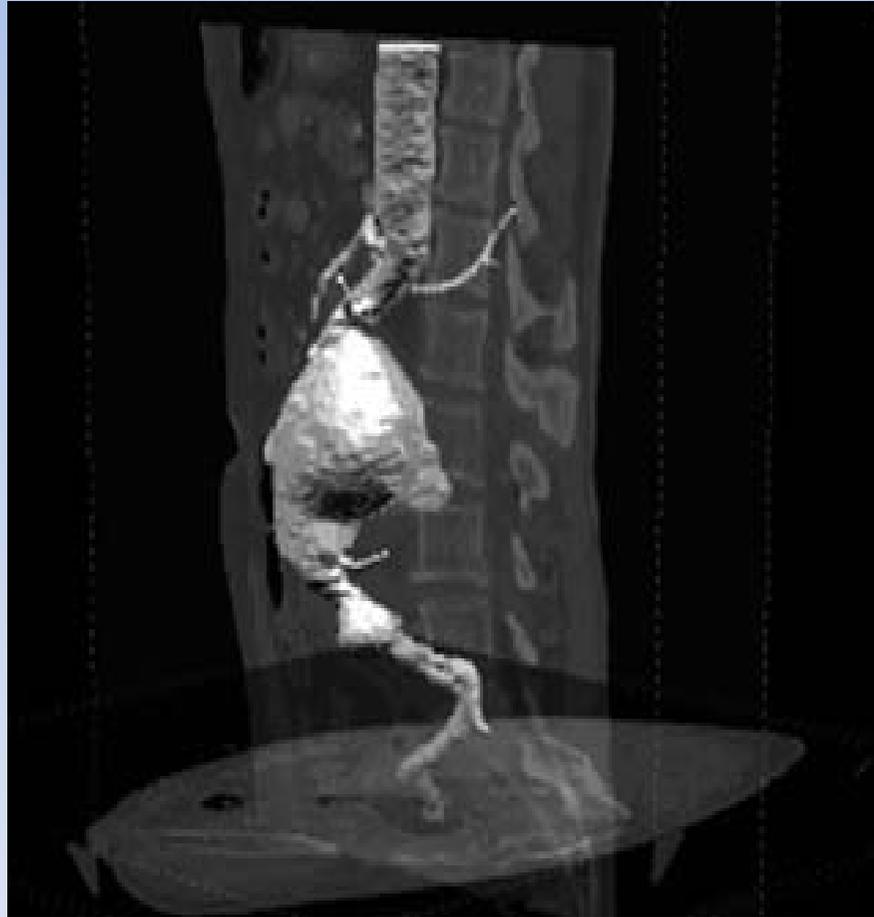
Unknown region

# GrabCut example

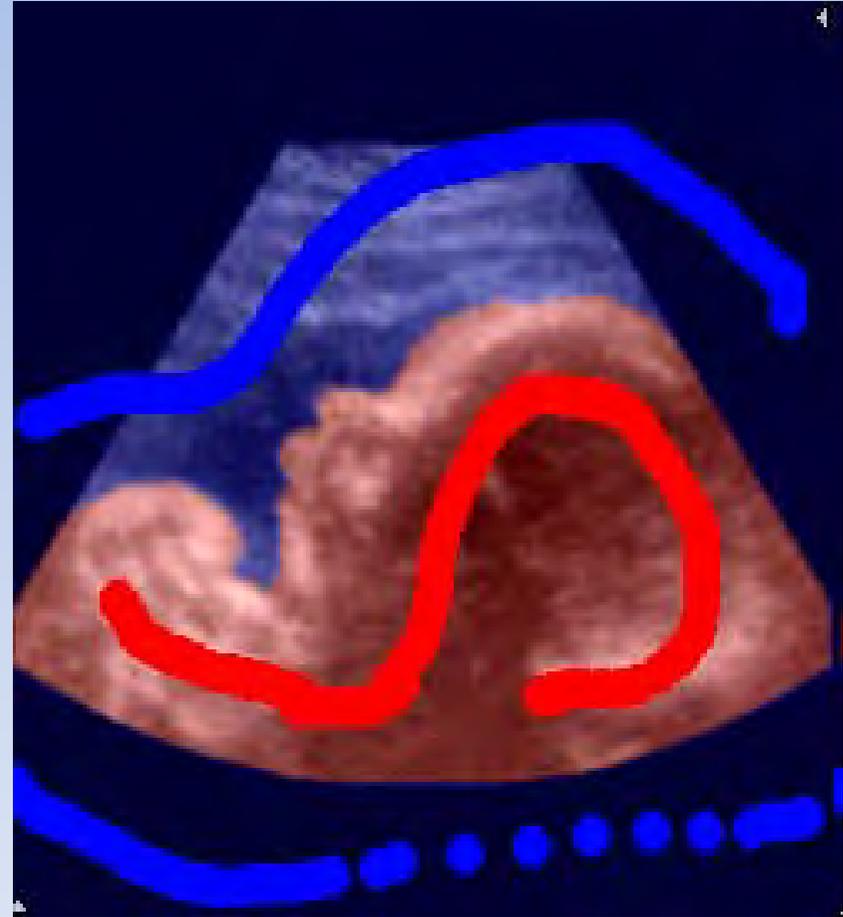
Foreground  
seeds



# Medical image graph-cut segmentation

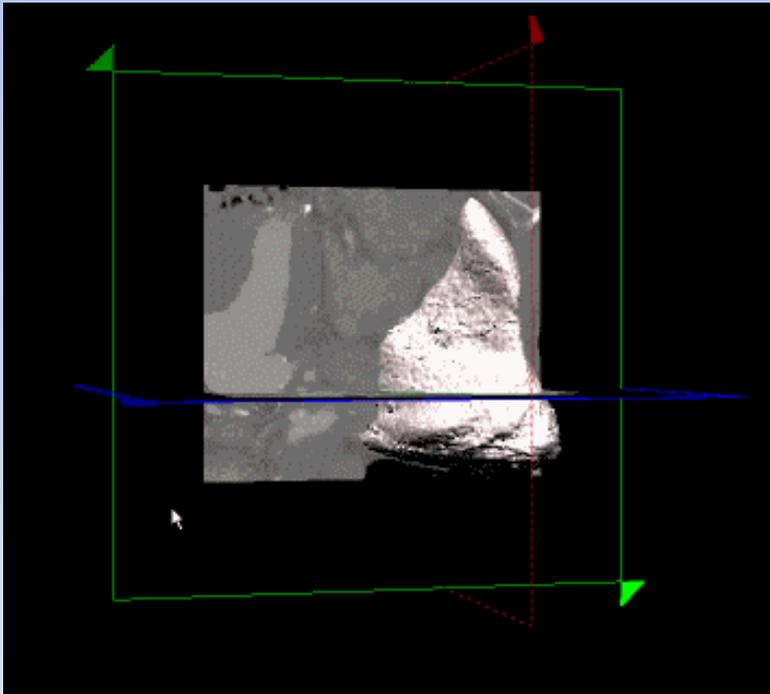


Abdomen segmentation

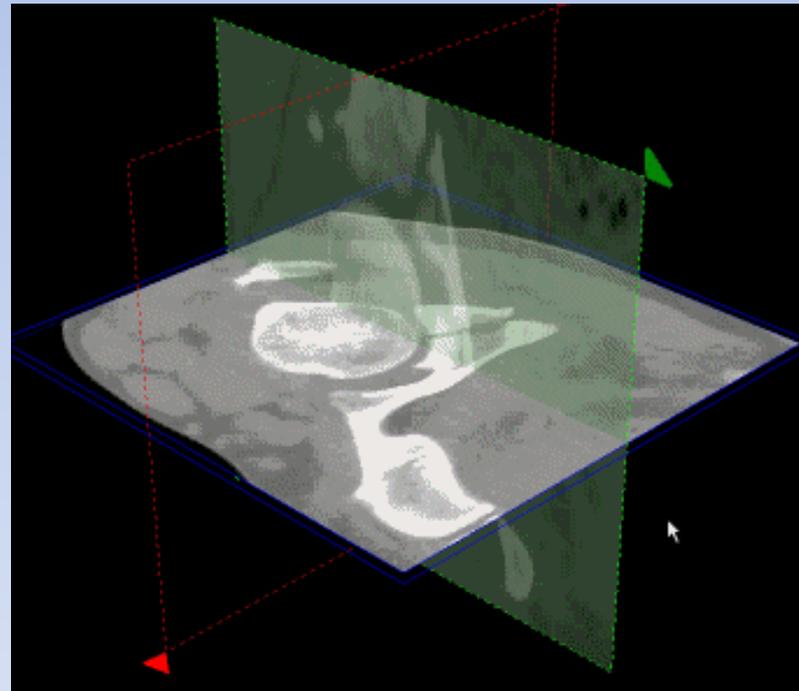


Baby segmentation

# Examples



Liver segmentation



Bone segmentation

# Conclusions

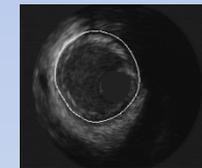
- **Fast and elegant region** segmentation method
- Assures the **global minimum** of the energy
- Needs **good cost** definition
- Grab cut is a natural extension to color segmentation of **multicolor** objects by GMM
- **Weak initialization** can help significantly to the segmentation

# Identify and compare the 4 deformable models

$$U(p) = \inf_{Q \in \mathcal{L}_p} \left\{ \int_Q P(Q) + \alpha \left| \frac{\delta Q}{\delta s} \right|^2 ds \right\}$$



$$E_{snake} = \int_0^1 E_{int}(u(s)) + E_{ext}(u(s)) ds.$$



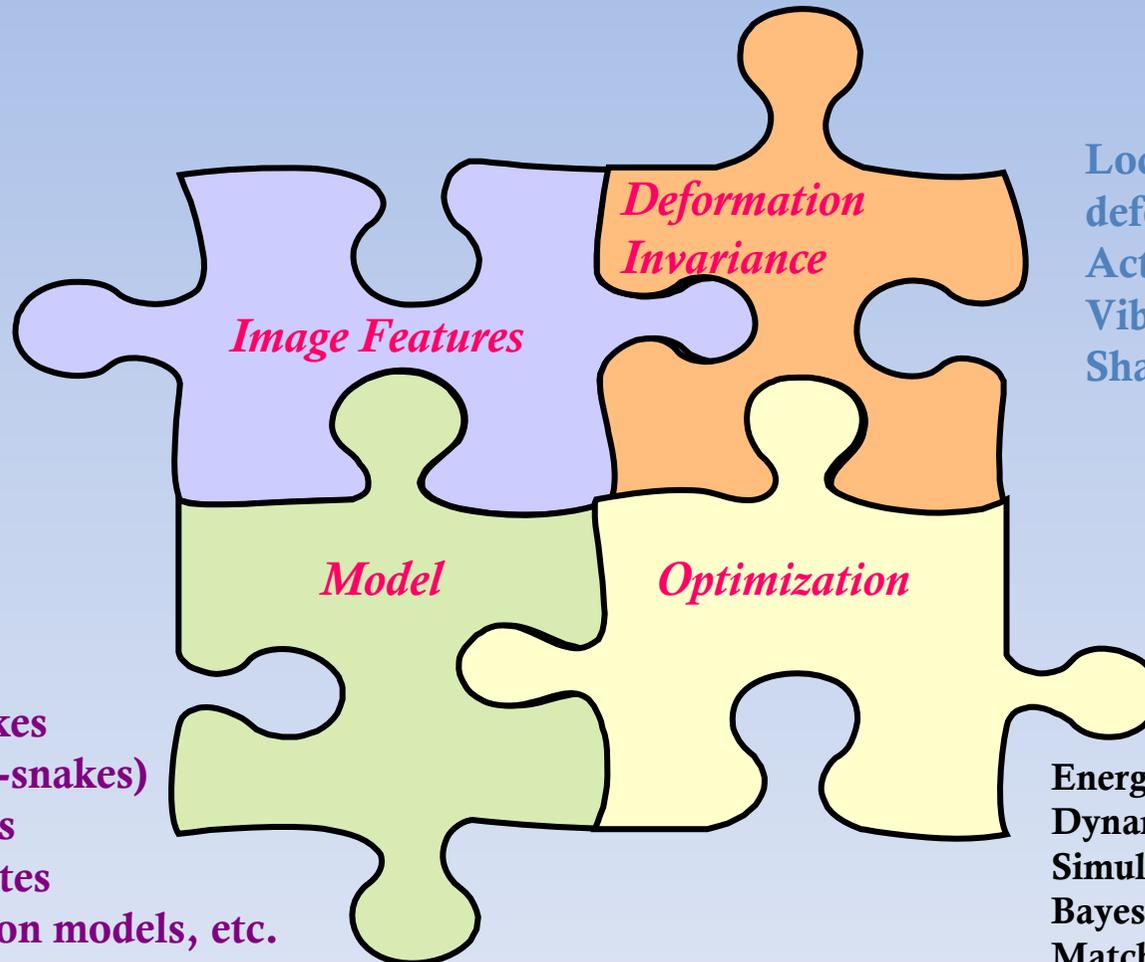
$$Q_t = g(I)(c + \kappa) \vec{n} - (\nabla g, \vec{n}) \vec{n}$$



$$E(L) = \sum_{p \in \mathcal{P}} D_p(L_p) + \sum_{(p,q) \in \mathcal{N}} V_{p,q}(L_p, L_q),$$

# Deformable Models “Unpuzzled”

Contour-based  
Region-based  
Texture-based  
Color-based  
Motion-based  
Stereo, etc.

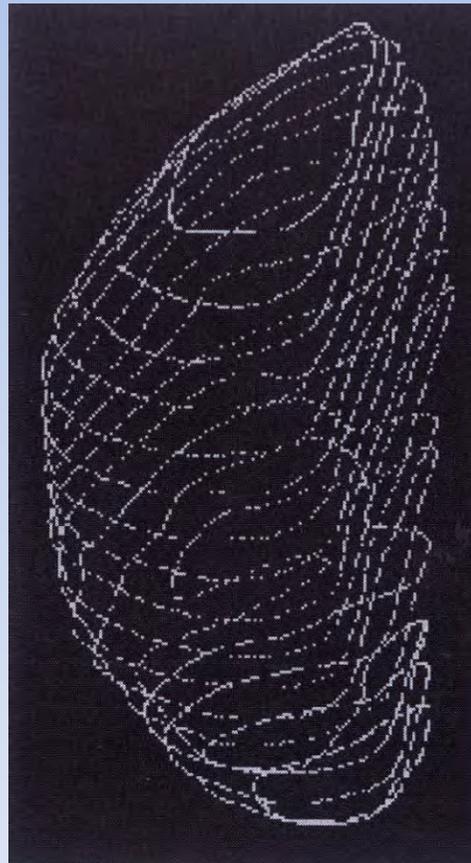
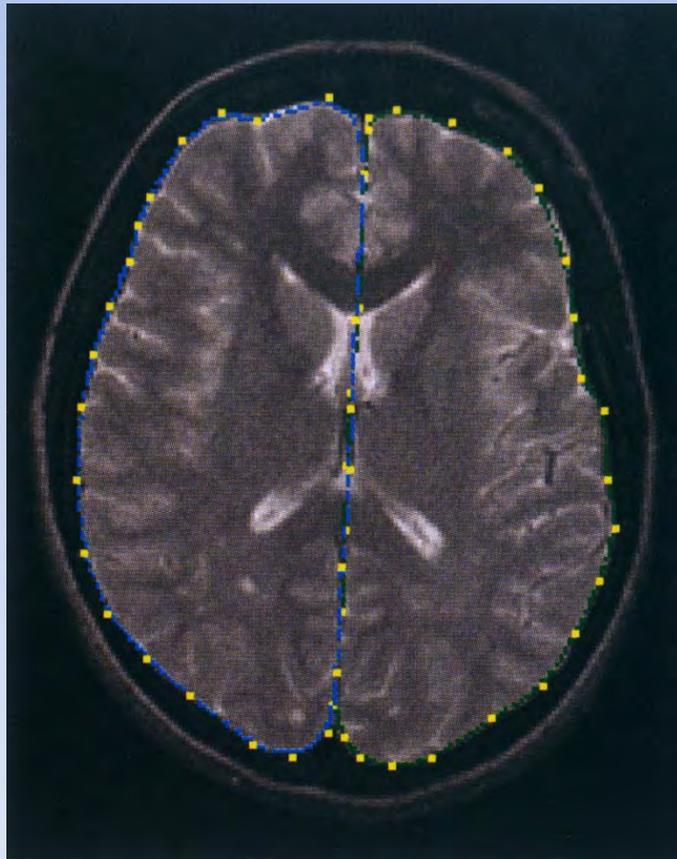


Local continuity deformations  
Active shape models  
Vibration modes  
Shape spaces

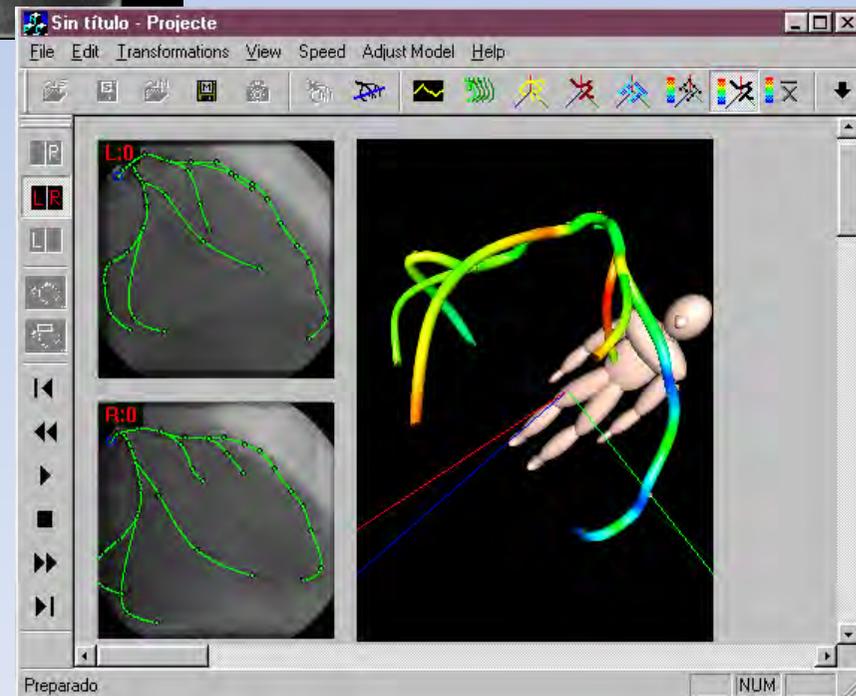
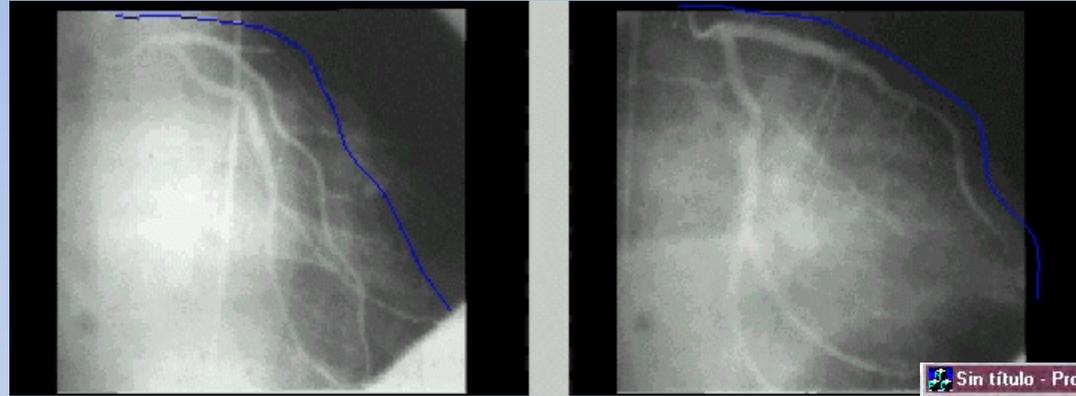
Parametric snakes  
(snakes, B-snakes)  
Geodesic snakes  
Flexible templates  
Point distribution models, etc.  
1D, 2D, 3D, 4D

Energy minimization  
Dynamic programming  
Simulated annealing  
Bayesian approach  
Matching  
Classification, etc.

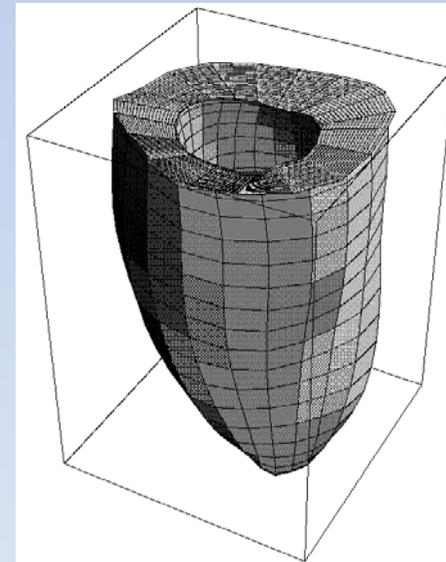
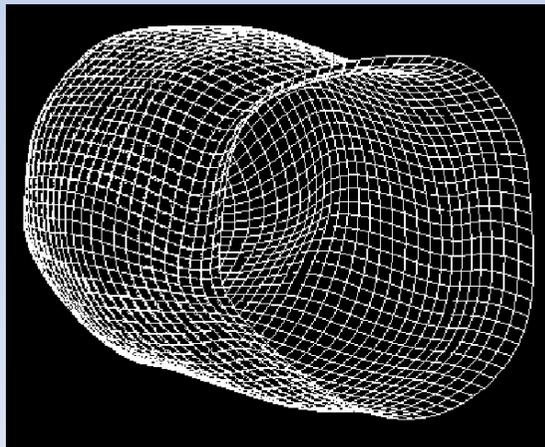
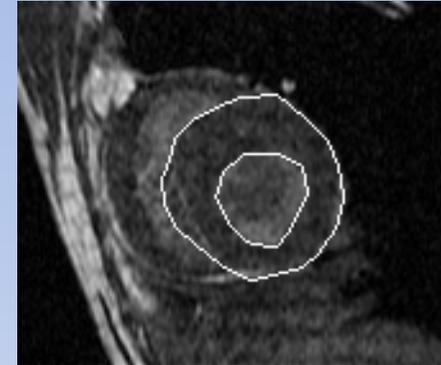
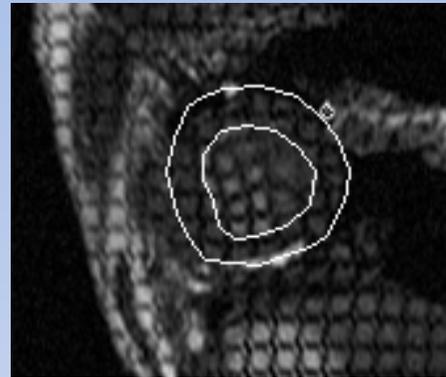
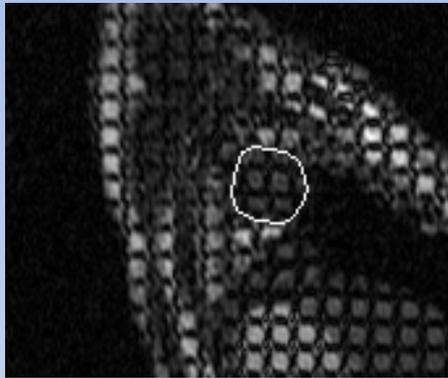
# Applications of deformable shapes



# Applications of deformable shapes



# Applications of deformable shapes

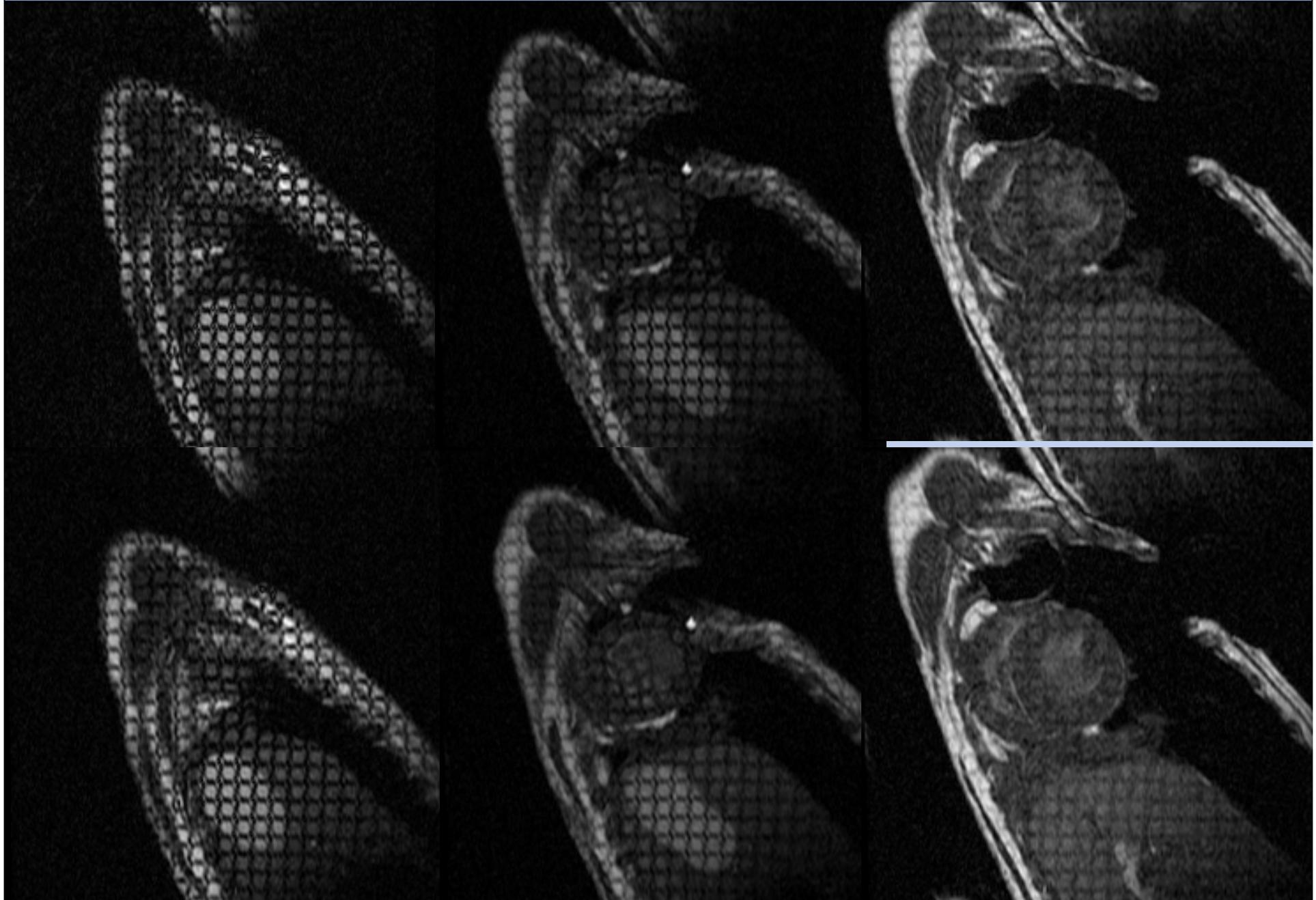


Level sets

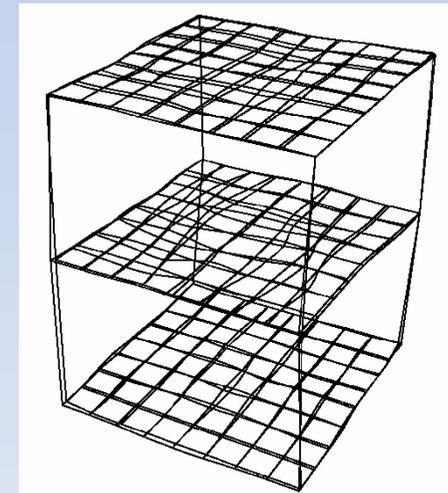
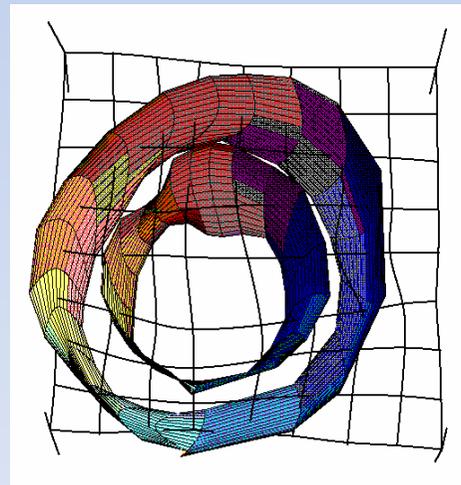
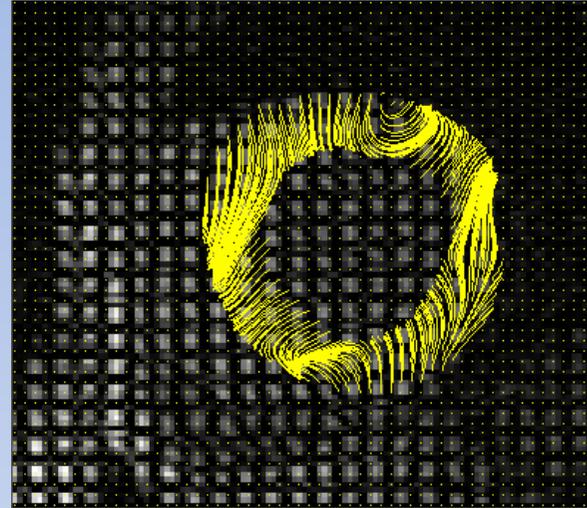
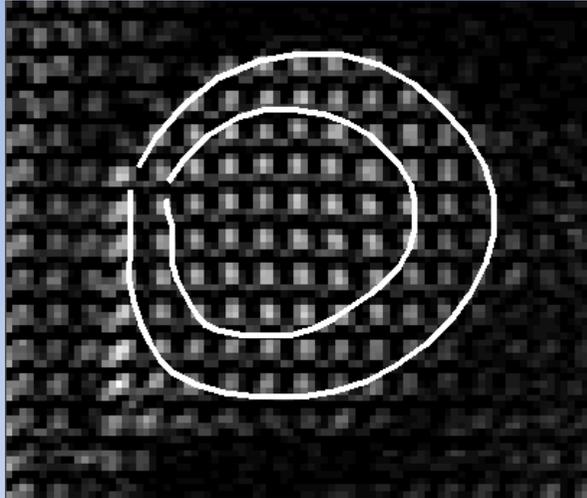
Fast marching

Graph cuts

**Applications**

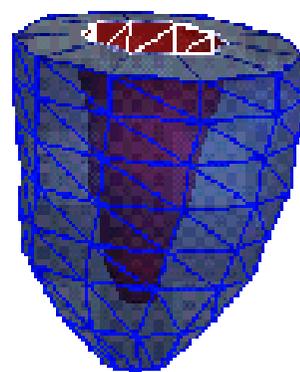
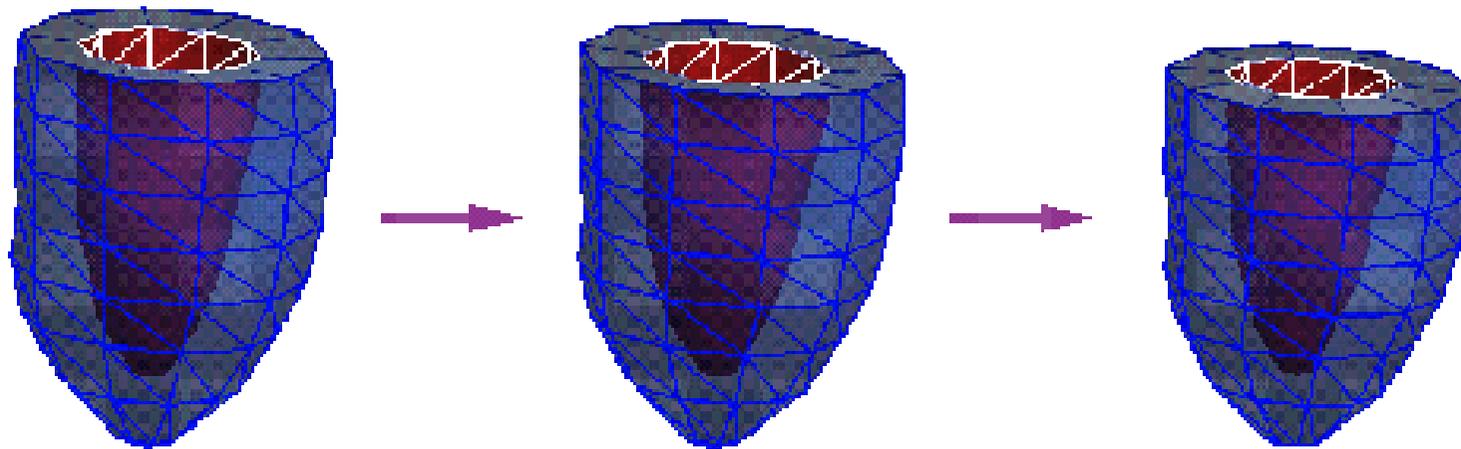


# Applications of deformable shapes

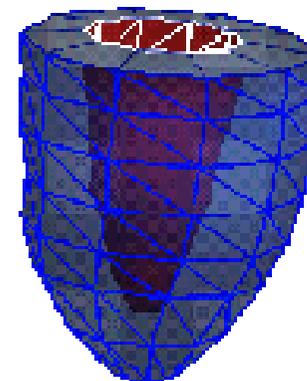


# Left Ventricle in Systole

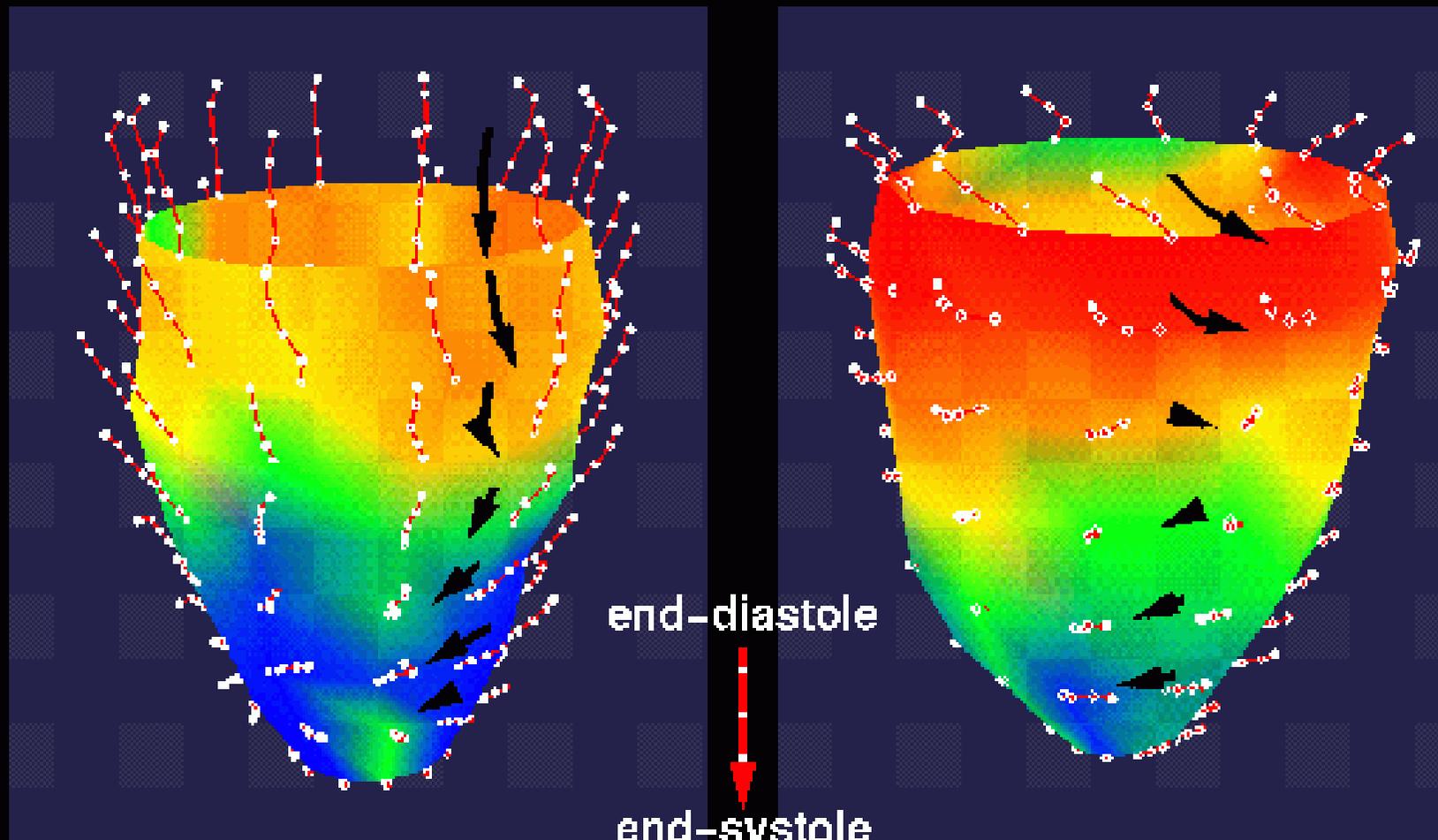
end-diastole



end-systole



# Twisting Motion of Left Ventricles during Systole



Normal

HTCM

counter-clockwise twist  $-10^{\circ}$   $0^{\circ}$   $+10^{\circ}$  clockwise twist

Thank you! 😊